

## **Mechanistic Drug Delivery Models**

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# **Disclaimer**



## *This presentation reflects the views of the author and should not be construed to represent FDA's views or policies.*

## *The presenter is offering his perspective based upon his experiences during regulatory decision-making*

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### **What Are the Drug Development Failure Modes?**

### **Research/Discovery**

- Ineffective disease target
	- Lack of efficacy
	- On target safety
- Ineffective design of drug molecule
	- Chemical, biologics, RNAs, and Gene therapies
	- Mechanism of action; off target effect
- Failed drug delivery
	- State of art formulation
	- Common challenge for oligonucleotide treatment

### **Development**

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• Wrong dose/dosing regimen/trial design













**Why 90% of Clinical Drug Development Fails and How to Improve It? STAR (Structure-Tissue Exposure/Selectivity-Activity-Relationship) Selects Better Drug Candidates and Balances Clinical Dose/Efficacy/Toxicity**

**II I High Dose Low Dose Low Success Best Success Rate High Rate Evaluate Class II Class I Most Desirable Specificity / Potency (SAR)** Specificity / Potency (SAR) **Cautiously Possible Successful Efficacy – Superior Efficacy – Adequate Possible Successful Examples: Toxicity – High Toxicity – Low Viagra, Sofosbuvir, Lipitor, Examples: Ibrutinib (I)? Remdesivir (IV)? Acalabrutinib, Tamoxifen, Spebrutinib (failed) Pomalidomide, Propranolol, Many Failed In Clinical Trials Famotidine, Clarinex, More III Class IV Class III IV Good Success Efficacy – Low Efficacy – Adequate Lowest Success Rate Toxicity – High Toxicity – Manageable Often Overlooked Rate Possible Successful Terminate Early Examples: Possible Successful**  Low **Thalidomide? Claritin? Tissue Exposure / Selectivity (STR)** High **Examples: Many Mistakenly Terminated Almost None Most Failed In Clinical Trials**  Sun D, et al. Acta Pharm Sin B. 2022. Slide Adapted from Dr. Duxin Sun

# Change Dosing vs Changing Delivery



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Change Dose/Dosing Regimen Change Drug Delivery



How to change drug delivery: API design, route of administration, and formulation **www.fda.gov**



# Drug Delivery Models

- Oral Absorption
- Orally inhaled
- Intranasal drug delivery
- Ophthalmic
- Topical dermatological
- Female reproductive tract/rectal/otic
- Oligonucleotide delivery (e.g., mRNA)

# **Concepts behind Complex Drug Products**

- Drug delivery systems include **GI Absorption, Inhalation, Intranasal, Topical Dermatological, Ocular/Otic, Transdermal, Intrarectal, Intravaginal/uterine, Parental, Long Acting Injectables, Implantable, Drug Device combiantions etc**
- **Complex Products** Under GDUFA
	- **Complex active ingredients**  Complex mixtures of APIs, polymeric compounds, peptides
	- **Complex formulations**  Liposomes, suspensions, emulsions, gels
	- **Complex routes of delivery**  Locally acting such as dermatological and inhalational drugs
	- **Complex dosage forms**  Long acting injectables and implantables, transdermals, MDIs
	- **Complex drug-device combinations**

#### **FDA FDA-Approved Pharmaceutical Products**



Zhong et al. Pharmaceutics. 2018 Dec; 10(4): 263

#### **Physiologically Based Models for Drug Delivery**

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**Recognize Critical Quality Attribute (CQA) for Ophthalmic Suspensions**

**Case 1**

#### Case study - Dexamethasone

- After instillation, several routes of dexamethasone transport:
	- Dissolved dexamethasone diffusing from tear film through cornea or conjunctiva
	- Solid particles and dissolved dexamethasone cleared from eye surface through co-> systemic circulation
- OCAT Model Development internally conducted rabbit study with PK sampling from multiple ocular tissues and plasma
- Model Verification with multiple datasets showing:
	- Particle size impact on ocular absorption
	- Viscosity impact on ocular absorption
	- Non-linear dose-exposure relationship



LeMerdy, Maxime, et al. "Application of Mechanistic Ocular Absorption Modeling and Simulation to Understand the Impact of Formulation Properties on Ophthalmic Bioavailability in Rabbits: A Case Study using Dexamethasone Suspension." The AAPS Journal 21.4 (2019): 65

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**SOLUTION** 

**SOLID** 

### **Case 1 Summary**

#### **Recognize Critical Quality Attribute (CQA) for Ophthalmic Emulsions**

#### Case study – Dexamethasone (cont'd)





Parameter sensitivity analysis in rabbit on PS and viscosity

- Viscosity is a critical attribute affecting BE
- Plasma/systemic PK is not reflective of local concentrations

Saturated solution vs. suspension simulations

- Solid particles in formulation leads to higher aqueous humor concentrations, BUT …
- Also higher systemic exposure
- A tool for product development that can weigh benefits and risks

LeMerdy, Maxime, et al. "Application of Mechanistic Ocular Absorption Modeling and Simulation to Understand the Impact of Formulation Properties on Ophthalmic Bioavailability in Rabbits: A Case Study using Dexamethasone Suspension." The AAPS Journal 21.4 (2019): 65

Le Merdy, Maxime, et al. "Physiologically based pharmacokinetic model to support ophthalmic suspension product development." The AAPS journal 22.2 (2020): 1-10.

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#### **Dermal PBPK Model to Supporting Diclofenac Sodium Topical Gel, 1% Approval**





· Blood flow

- Diclofenac sodium topical gel, 1%
- Alternative BE approach for a Q1/Q2/Q3 formulation: dermal PBPK model supported alternative to in vivo comparative clinical endpoint BE study
- Model development:
	- o API physicochemical properties
	- o API ADME properties
	- o Formulation attributes for Reference and Test drug products (e.g., viscosity, globule size, pH)

API: active pharmaceutical ingredient; ADME: absorption, distribution, metabolism, and elimination

#### **Dermal PBPK Model to Supporting Diclofenac Sodium Topical Gel, 1% Approval**



- Platform performance assessment:
	- o >10 PBPK models for TDS and topical products
	- o Multiple doses/product strengths and dosing regiments
	- Satisfactory model performance
- Model performance assessment for diclofenac sodium topical gel, 1%:
	- o Literature and application data on doses, product strengths, dosing regiments, routes of administration and local/systemic exposure data
	- o Formulation attributes for R and T
	- o Good predictions of systemic exposure

R: Reference, T: Test, TDS: Transdermal Delivery System

Tsakalozou et al. CPT Pharmacometrics Syst Pharmacol. 2021 Feb 6. doi: 10.1002/psp4.12600

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#### **Dermal PBPK Model to Supporting Diclofenac Sodium Topical Gel, 1% Approval**



- Refined model to improve synovial fluid exposure predictions (by the Agency)
	- o Protein binding in all skin layers
	- o Drug product attributes updated
	- o Partition coefficients modified leveraging observed local drug amounts

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**Dermal PBPK Model to Supporting Diclofenac Sodium Topical Gel, 1% Approval**

- Conducted virtual BE assessments on predicted systemic and local exposure data
- Sensitivity analysis to check on effect of changing parameters values on conclusion
	- ✓ **R and T drug products were found bioequivalent**



R: Reference, T: Test

Tsakalozou et al. CPT Pharmacometrics Syst Pharmacol. 2021 Feb 6. doi: 10.1002/psp4.12600





**Dermal PBPK Model to Supporting Diclofenac Sodium Topical Gel, 1% Approval**

- First case for using PBPK model to directly approve a product.
- PBPK models can be used to inform product development decisions and support alternative BE approaches for generic locally-acting drug products.
- Applicants are encouraged to follow best practices when developing PBPK models for generic locally-acting drug products as these are communicated by the Agency in guidances and other public forums.
- Applicants are encouraged to engage with the Agency early in their product development program by making use of the pre-ANDA meeting request program (GDUFA III).

## **Case 3: Targeting Central Nervous System (CNS) Delivery with Nasal Drug Products (NDPs)**

- Treat CNS disorders without the need to overcome the blood-brain-barrier
- Reduce dose needed and possibly increase rate of delivery
- Many treatments are in development
	- Alzheimer's Disease
	- Parkinson's Disease
	- Migraines

## **Case 3: Nasal Drug Products (NDPs) with Olfactory Targeting Claims**



- Trudhesa® (dihydroergotamine mesylate nasal spray)
	- Approved September 2, 2021
	- Indicated for treatment of migraines
	- Olfactory targeting not specified on product label
- **Precision Olfactory Delivery®** system $1$ 
	- Large or small molecules, liquid or powder, to upper nasal cavity or upper turbinates
- Onzetra Xsail® (sumatriptan succinate nasal powder)
	- Approved January 27, 2016
	- Indicated for treatment of migraines
	- Olfactory targeting not specified on product label
- Optinose<sup>®</sup> system<sup>2</sup>
	- Aims to deliver deep into nasal cavity
	- Hypothesis that there may be local uptake via olfactory and trigeminal nerves

2. Cady et al. Headache: The Journal of Head and Face Pain. 2015;55(1):88-100.

<sup>1.</sup> Shrewsbury et al. Headache: The Journal of Head and Face Pain. 2019;59(3):394-409.

## **Nose-to-Brain Drug Delivery**



Agrawal et al. Journal of controlled release. 2018;281:139-77.

### **Case 3: Bioequivalence (BE) at the Site of Action for Locally-Acting NDPs**

- For locally-acting NDPs, nasal tissue is the site of action
- Regional deposition is upstream of local tissue drug exposure and systemic pharmacokinetics (PK) is downstream



Liu et al. Journal of applied physiology. 2009;106(3):784-95.

## **Case 3: Weight of Evidence Approach for Locally-Acting Nasal Sprays**



BE recommendations include in vitro studies, in vivo studies, and formulation and device sameness



21 U.S. Food and Drug Administration Draft Guidance for Industry: Bioavailability and Bioequivalence Studies for Nasal Aerosols and Nasal Sprays for Local Action



## **Case 3: Quantification of Drug Delivery to Brain**

- Receptor binding in brain may be quantified using positron emission tomography (PET) scan data
	- Ethical concerns with conducting BE study
- Alternative BE approach?
	- Combination of in vitro and/or silico studies
	- Can modeling be used to design such an approach?



#### Percent of maximum receptor binding value from PET scan data

Fowler and Volkow. Journal of Toxicology: Clinical Toxicology. 1998;36(3):163-74

## **Case 3: Computational Fluid Dynamics (CFD) Modeling of NDPs**

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- Predict influence of device and formulation parameters
	- Particle size distribution, spray angle, spray velocity
	- Regional deposition
		- Intersubject variability
	- PK profile
		- Combined with physiologicallybased pharmacokinetic (PBPK) modeling



Fiber deposition in nasal cavity, where a is the fiber radius in µm, β is the fiber aspect ratio, IP is the impaction parameter, and DF is the deposition fraction. (Fig. 13 from Dastan et al)

## **Case 3: PBPK Modeling of NDPs**



Nasal PBPK model structure as shown in Fig. 2 of Andersen et al.

### • Compartmental model

- Prediction of local and systemic PK
	- Dissolution in mucus layer
	- Absorption through nasal tissue
	- Metabolism in nasal tissue
	- Integration with systemic model
- Validated with in vivo PK data

Andersen et al. Regulatory Toxicology and Pharmacology. 2002;36(3):234-45

### **Modelers' Way to Understand the Scheme**



## **Case 3: Fully 3D Nasal Mucociliary Clearance (MCC) Model**





Nasal MCC model features, including a) 6 mm/min mucus velocity vectors in mucus layer and b) regional definitions including olfactory (red), nasal vestibule (blue), and nasal cavity (orange) regions. (Fig. 1 of Chari et al)

- North Carolina State University
	- PI: Clement Kleinstreuer
	- Grant #1U01FD006537: 2018-2021
- 3D CFD model is used to predict regional deposition of NDPs
- Particle deposition locations are directly translated to fully 3D mucus layer model
- Nasal MCC model predicts transit, dissolution, and absorption simultaneously
	- Can be used for predicting olfactory region deposition and absorption

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Chari et al. Journal of Aerosol Science. 2021;155:105757.

## **Case 3: Fully 3D Nasal MCC Model - Results**

- Model sensitivity was investigated
	- Oil-in-water partition coefficient  $(K_{o/w})$
	- Solubility (C<sub>s</sub>)
	- Particle diameter (d)
- High values of  $K_{o/w}$  and  $C_s$  produced rapid absorption
- Smaller particles show initial burst in absorption rate, but after burst, rates are similar
- Effect of deposition locations was investigated



Mucus layer drug concentrations for drug with  $K_{\text{o/w}} = 0.005$ ,  $C_s =$ 0.02 mg/mL, and  $d = 5 \mu m$  for regional depositions ratios in the nasal vestibule and nasal cavity regions of a) 80/20, b) 50/50, and c) 20/80. (Fig. 15 of Chari et al)

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## **Case 3: Nasal In Vitro Models**

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Cut-open view of the left nasal passage



Cut-out olfactory region (OL)



Nasal in vitro model that allows for measurement of olfactory region deposition. (Adapted from Fig. 1c of Xi et al.)

- Drug product is actuated into nasal model
- Deposited drug is measured from removable sections using high performance liquid chromatography (HPLC)
- Deposition may show significant intersubject variability according to anatomical differences
- Olfactory deposition may be measured with separate section

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Xi et al. Journal of aerosol medicine and pulmonary drug delivery. 2017;30(2):118-31.

# **Case 3 Summary**



- 1. Nose-to-brain drug delivery is an emerging area for product development.
- 2. Modeling may be used with relevant in vitro studies to develop an effective toolset to characterize nose-to-brain drug delivery.
- 3. Further work using PBPK models to address noseto-brain pathways needed to facilitate their use.

# **Case 4: Nanoparticles (NPs)**



- Drug delivery cannot be determined based on systemic pharmacokinetics (NP properties + tissue properties)
- Multi-scale models to characterize drug distribution at each scale (eg, body, tissue, cellular, and sub-cellular)
	- Endocytosis at cellular level
		- 100-150 nm: Clathrin-mediated endocytosis
		- 50-100 nm: Caveolae-mediated endocytosis is used by smaller NP
		- 40-50 nm: Clathrin- and caveolae-independent endocytosis
	- Other non-receptor or receptor mediated internalization mechanisms
- Model based identification of key factors for NP drug delivery

# **Case 4: Mathematical Models**





The variables and their initial values used in the above equations are described in Table 1. The model contains nine parameters obtained from direct experimental measurements and published literature, 18, 22, 23, 24, 25 as illustrated in Table 1. We modeled these differential equations in the Simbiology toolbox developed for MATLAB users (code is included in the Supplemental Information; The Mathworks).

# **Case 4: Summary**



- Current NP delivery models focus on characterizing what is going on with a formulation but cannot decide what formulation parameter can change delivery
- Future models can be more mechanistic to discover critical quality attributes for NP drug deliveries



## A Computational Theory for PBPK



Route with Tumor Visits

Route 1

Route 2

Route 3

**How to mathematically describe this decomposition?**

#### **Matrix Convolution Expansion in a Linear System**

**Theorem 1** In a linear n-compartment system, the probability matrix for a drug molecule to travel from one compartment to another with m inter-compartment transitions after an elapsed time t can be expressed as

$$
\mathbf{P}^{m}(t) = ((\mathbf{P}^{0} \cdot \mathbf{K}')^{*m} * \mathbf{P}^{0})(t), \qquad (8)
$$

where  $*$  is the matrix convolution operator,

$$
\mathbf{K}' = \begin{bmatrix} k_{11} & \cdots & k_{1n} \\ \vdots & \ddots & \vdots \\ k_{n1} & \cdots & k_{nn} \end{bmatrix} - \text{Diag}(k_{11}, \ldots, k_{nn}) = \begin{bmatrix} 0 & \cdots & k_{1n} \\ \vdots & \ddots & \vdots \\ k_{n1} & \cdots & 0 \end{bmatrix}, \qquad (9)
$$

and

$$
\mathbf{P}^{0}(t) = \text{Diag}\left(e^{k_{11}t}, e^{k_{22}t}, \dots, e^{k_{m}(t)}\right).
$$
 (10)

$$
\mathbf{P}(t) = \sum_{m=0}^{\infty} \mathbf{P}^{m}(t) = \sum_{m=1}^{\infty} ((\mathbf{P}^{0} \cdot \mathbf{K}')^{*m} * \mathbf{P}^{0})(t)
$$

### **Concept behind the Calculations of a Compartment Model**





$$
P_{12}^{3}(t) = K_{12}K_{21}K_{12}P_{11}^{'}(t)*P_{22}^{'}(t)*P_{11}^{'}(t)*P_{22}^{'}(t)
$$
  
+  $K_{13}K_{31}K_{12}P_{11}^{'}(t)*P_{33}^{'}(t)*P_{11}^{'}(t)*P_{22}^{'}(t)$   
+  $K_{12}K_{23}K_{32}P_{11}^{'}(t)*P_{22}^{'}(t)*P_{33}^{'}(t)*P_{22}^{'}(t)$ 

### **Computational Solutions: Conventional Solution vs Matrix**

### **Convolution Expansion Method**

 $k12 = 0.75$ ; k13 = 1.2; k10 = 0.95;  $k21 = 3.2$ ;  $k23 = 1.1$ ;  $k31 = 1.2$ ;  $k32 = 0.6$ 

#### **Solution based on conventional PK method**

 $P_{11}(t) = 0.29e^{-5.3t} + 0.37e^{-3.35t} + 0.34e^{-0.38t}$ 



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#### **Solution based on convolution expansion approach**  (only up to 7 inter-compartment transitions are used)

$$
P_{11}(t) \approx (-19.35 - 10.30t - 1.20t^{2})e^{\sqrt{4.3}} + (-4.45 - 25.74t + 7.76t^{2} - 0.16t^{3})e^{\sqrt{2.3}t} + (24.80 - 18.30t + 5.06t^{2})e^{\sqrt{1.3}t}
$$
  
\nk21+k23=3.2+1.1=4.3  
\nk12+k13+k10 = 0.75+1.2+0.95 = 2.9  
\n**Significance for**  
\nk31+k32=1.2+0.6=1.8  
\n**Styair**

## **Utilities of Matrix Convolution Expansion**



- Decompose observed drug exposure to summation of drug molecules following all traveling routes
- Can compute target site drug exposure
- Can compute residence times at the target site
- Can compute many other fine details

# **Overall Summary**



- Unprecedented opportunities for using PBPK models to inform drug delivery and formulation design
- Broadening value proposition of mechanistic modeling from perspectives of drug delivery
- Call for next generation modelers and drug developers with forward looking vision
	- Post Lewis Sheiner era
	- Go early Go mechanistic!

# Acknowledgement

- Case Contributors
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- ORS/OGD
	- Robert Lionberger, PhD
	- Lei Zhang, PhD

# backups



#### **FDA Case V: Long-Acting Injectable Drug Products**

- Long-acting injectable (LAI) drug products are formulated to achieve extended drug release action from days to years when administered via intramuscular, subcutaneous, intravitreal, or other routes.
- These products can help improve patient compliance with a better therapeutic option to treat patients who adhere poorly to frequently administered medication.

## **Examples of FDA Approved LAI Drug Products and Approved ANDAs**





## **Challenges in LAI Product Development and Lifecycle Management**

- Long apparent half-life:
	- Longer time to reach steady state
	- Longer wash out time
	- Longer duration for bioequivalence (BE) studies
	- High drop out rate
	- Not practical to perform a singledose crossover BE study
- Challenging to propose relevant dosing scenarios, e.g.,
	- Impact of early, delayed or missed doses
	- Switching between formulations

## **Recent Examples of Population PK-MIE Virtual BE**



- Proposals for some oncology/orphan drugs in pre-ANDA meetings
- **Reduced sample size** and shorter duration in vivo PK studies
- MIE framework for LAIs by Uppsala University (GDUFA research)



## **Common Deficiencies in MIE VBE**



- The applicant did not submit a modeling analysis plan (MAP)
- The applicant did not evaluate the type I error before virtual BE simulation
- The model is not able to detect potential formulation difference between test and reference products
- The sample size of virtual BE simulation is a lot larger than the sample size of clinical BE study for model building without sufficient justifications
- The applicant did not understand that the model building and validation in BE decision is more stringent than the pop-PK modeling in new drug development.

## **Future Perspectives for LAI**

- Further cost saving via
	- Reduction in clinical study size and duration
	- Optimization of study design
- Improving simulation technique
	- Model averaging
	- Non model averaging
	- Bayesian method (Markov Chain Monte Carlo)?
- Model validation
	- Population PK guidance
	- Additional considerations for MIE BE
- Model sharing, submission, communication
	- Model Analysis Plan
	- Model Master Files