

An Integrated Multiscale-Multiphysics Modeling of Ocular Drug Delivery and Pharmacokinetics pharmacological protection and treatment

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**PPBPK Modeling for The Development and Approval of
Locally Acting Drug Products
ASCPT 2019 Annual Meeting**

Washington DC, March 13, 2019

Develop the multiscale computational framework, CoBi, for modeling **in vitro and in vivo** ocular drug delivery, PK/PD and to establish protocols for model-based assessment of BE of generic drugs.

- **Multiscale modeling tools dissolution of ophthalmic products**
- **Modeling of Dissolution Devices and Protocols**
- **Improves of the Anterior Eye Model**
 - **Anatomic Geometry**
 - **Tear Film**
 - **Models of Topical Delivery of Suspension Products**
- **Validation of the Corneal Model on Iv Vitro data**
- **Whole Eye Model Q3D – 3D**
- **Simulation of Timolol PK – PD**
- **Posterior Eye Model**

Acknowledgements:

FDA: Dr. Andrew Babiskin, Dr. Ross Walenga, Dr. Jianghong Fan

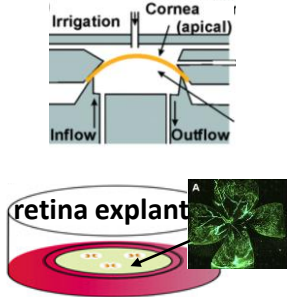
CFDRC: Dr kay Sun, Mr Joseph Pak, Dr ZJ Chen

Supported by FDA. FDA/OGD (5U01FD005219-02, HHSF223201810151C)

Overview

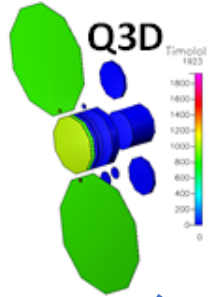
High-Resolution Ocular Models

In Vitro/Ex Vivo Validation

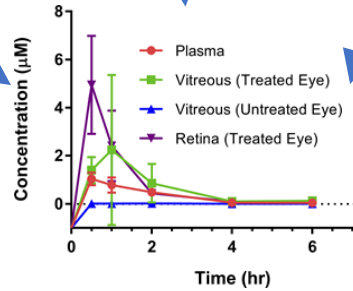
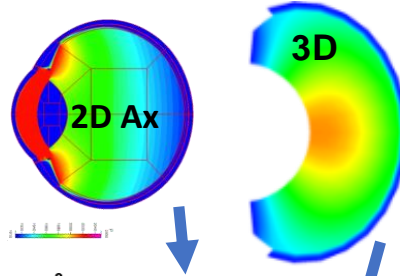


In Vivo Validation

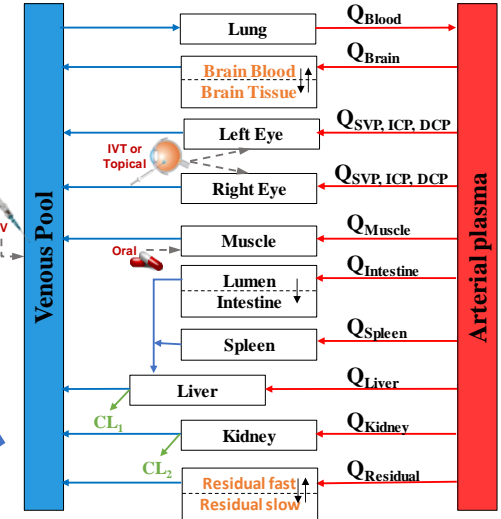
Anterior Eye



Posterior Eye

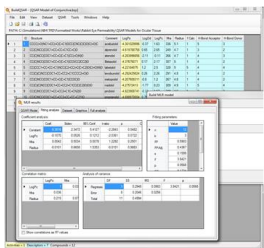


PBPK Whole-Body Model

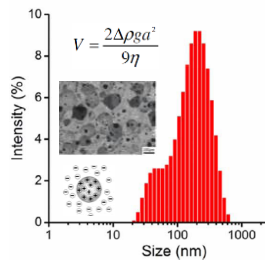


Formulation Properties

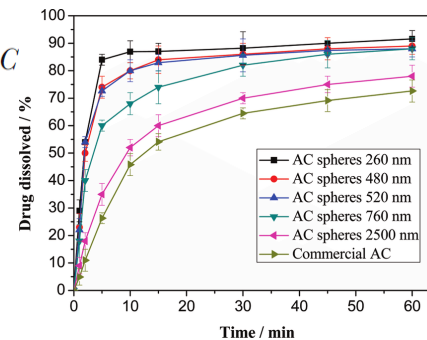
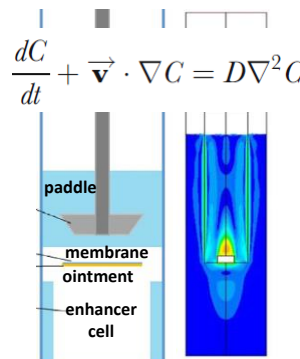
Biochemical



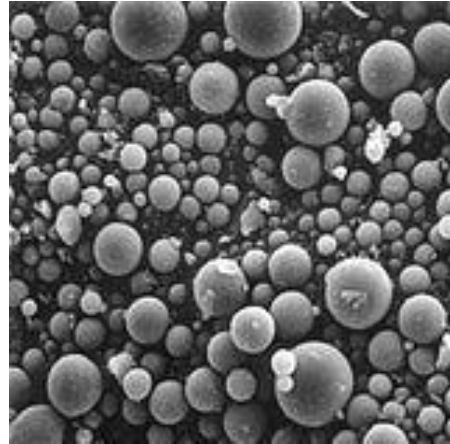
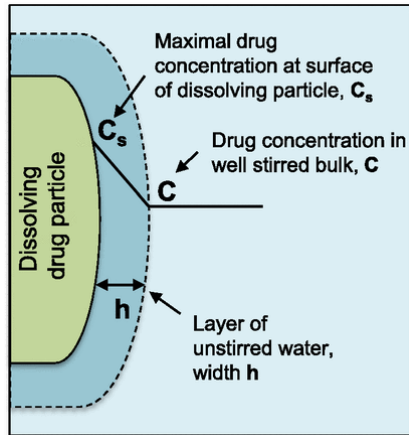
Biophysical



Dissolution Model



Solid Particles



Dissolution: Change in Particle Mass

$$\frac{dM_p}{dt} = -D \cdot A \cdot (C_s - C_b) \cdot \left[\frac{1}{h} + \frac{1}{R} \right]$$

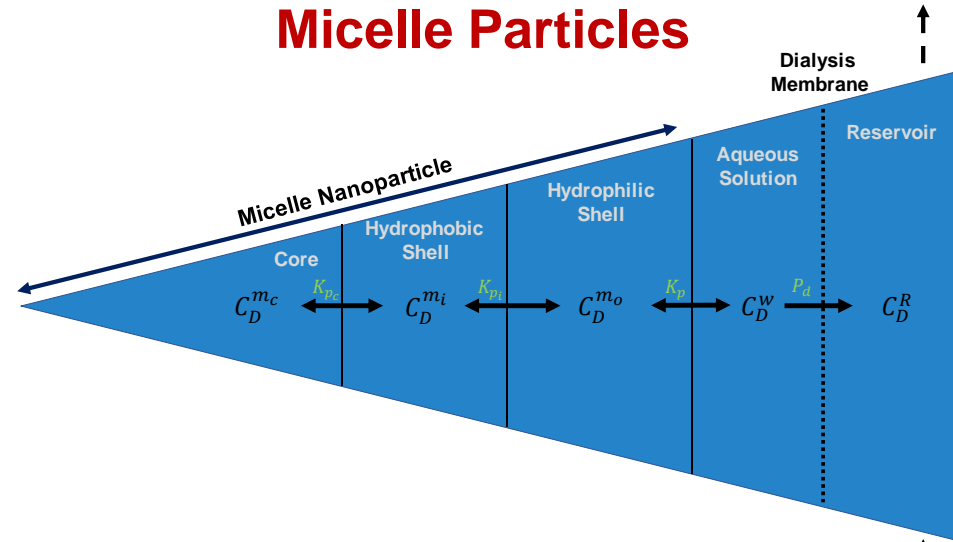
Change in Particle Radius

$$r_{p,i} = \left(\frac{3}{4\pi} \cdot \frac{M_{p,i}}{N_i \cdot \rho} \right)^{1/3}$$

Dissolution: Change in Bulk Media Conc.

$$\frac{dC_b}{dt} = \frac{D \cdot A}{V_{media}} \cdot (C_s - C_b) \cdot \left[\frac{1}{h} + \frac{1}{R} \right] \cdot N_i$$

Micelle Particles



$$V_{m_c} \frac{dC_D^{m_c}}{dt} = -A_{p_c} P_{p_c} \left(C_D^{m_c} - \frac{C_D^{m_i}}{K_{p_c}} \right)$$

$$V_{m_i} \frac{dC_D^{m_i}}{dt} = A_{p_c} P_{p_c} \left(C_D^{m_c} - \frac{C_D^{m_i}}{K_{p_c}} \right) - A_{p_i} P_{p_i} \left(C_D^{m_i} - \frac{C_D^{m_o}}{K_{p_i}} \right)$$

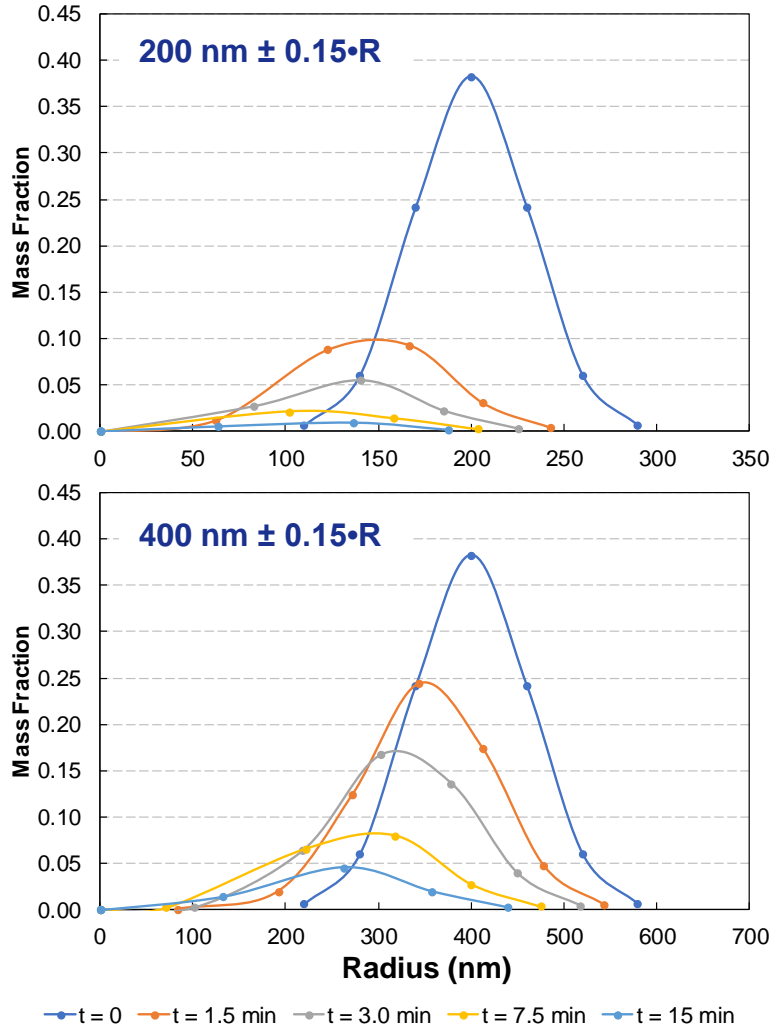
$$V_{m_o} \frac{dC_D^{m_o}}{dt} = -A_p P_p \left(C_D^{m_o} - \frac{C_D^w}{K_p} \right) + A_{p_i} P_{p_i} \left(C_D^{m_i} - \frac{C_D^{m_o}}{K_{p_i}} \right)$$

$$V_w \frac{dC_D^w}{dt} = A_p P_p \left(C_D^{m_o} - \frac{C_D^w}{K_p} \right) - A_d P_d (C_D^w - C_D^R)$$

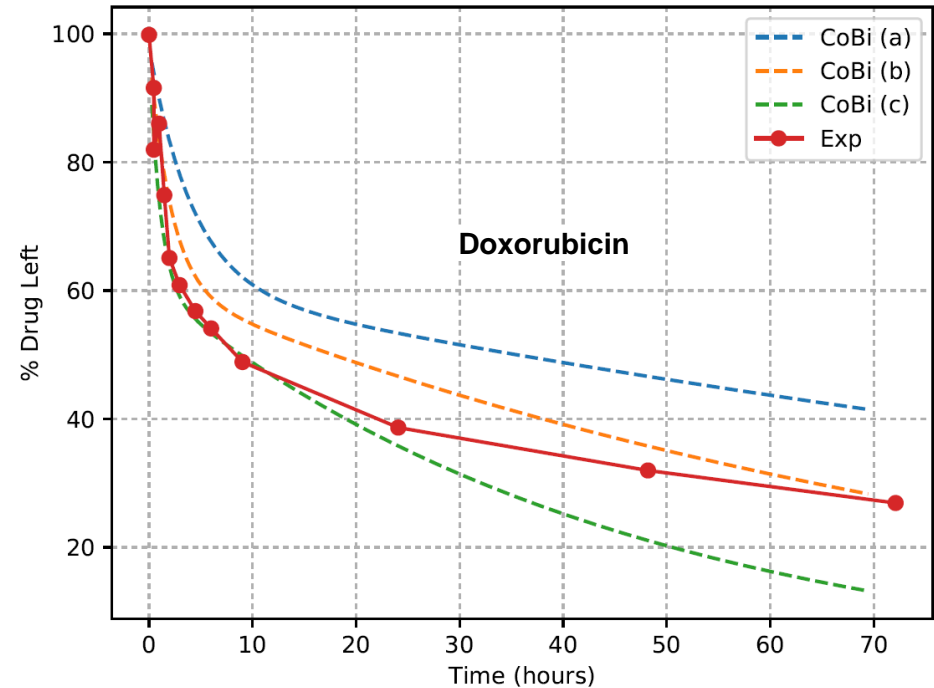
$$V_R \frac{dC_D^R}{dt} = Q_{R,in} (C_{D,in}^R - C_D^R) + A_d P_d (C_D^w - C_D^R)$$

Dissolution Models: Particle Suspensions

Solid Particles



Micelle Particles

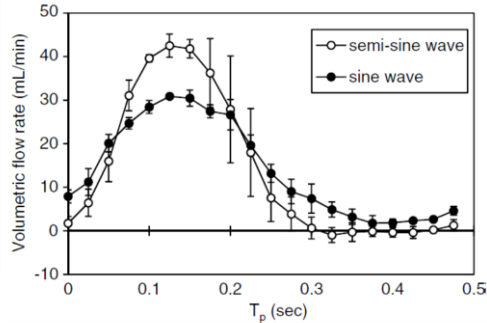
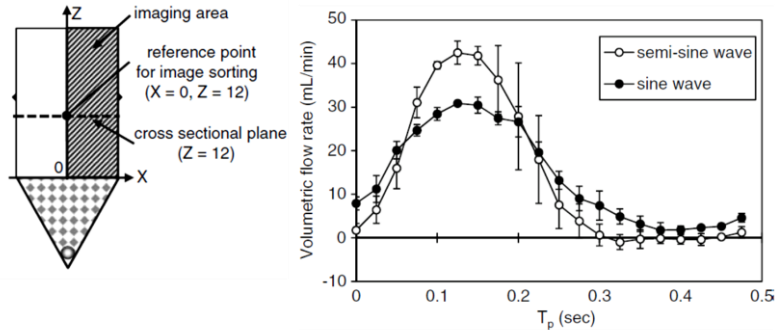


Calibration Parameters

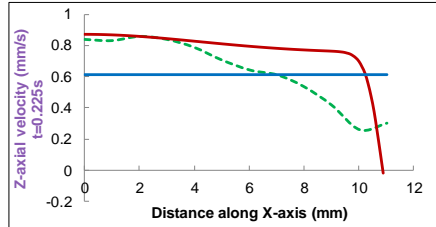
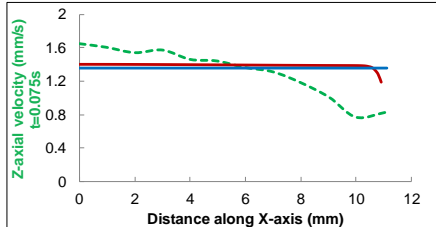
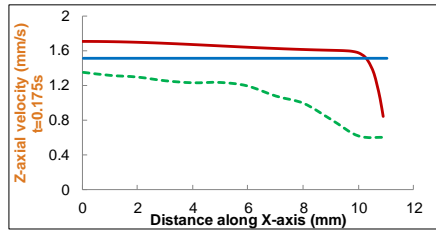
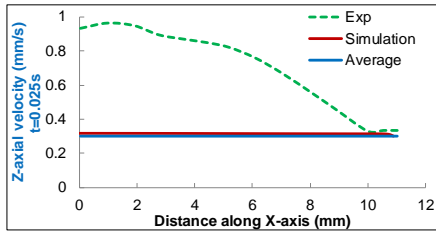
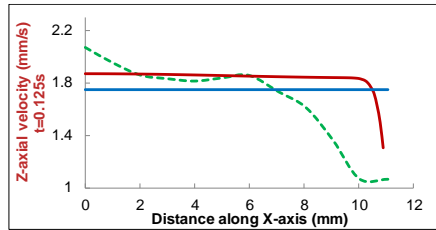
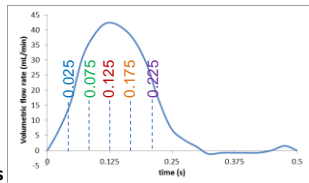
	$k_s (\times 10^{-2} h^{-1})$	$k_f (h^{-1})$
(a)*	0.55	0.24
(b)	1.1	0.48
(c)	2.2	0.96

Dissolution Models: In Vitro Systems

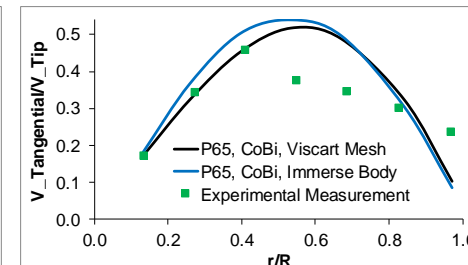
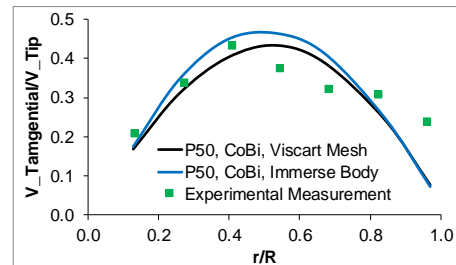
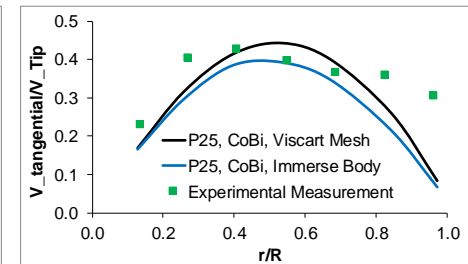
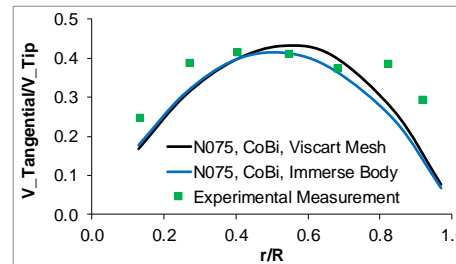
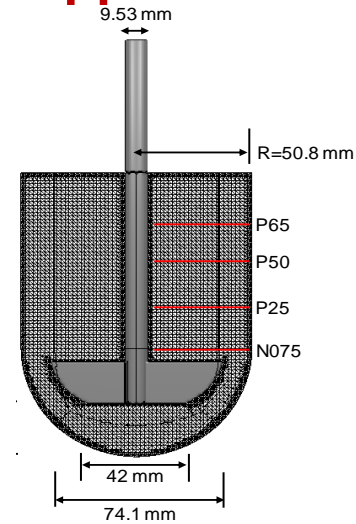
USP 4 Apparatus



Discharge:
 $t=0.025$ to $0.225s$



USP 2 Apparatus

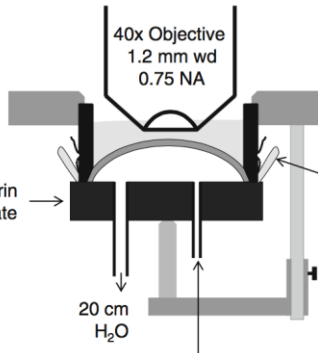


H. Yoshida, et al Effects of Pump Pulsation on Hydrodynamic Properties and Dissolution Profiles in Flow-Through Dissolution Systems (USP 4),” *Pharm. Res.*, vol. 33, no. 6, pp. 1327–1336, 2016.

G. Bai, P. M. Armenante, et al. Hydrodynamic investigation of USP dissolution test apparatus II, *J. Pharm. Sci.*, 96(9)2327–2349, Sep. 2007 6

In Vitro/Ex Vivo Modeling Approach

Experimental Setup



Tear and AH baths had the same volume:

$$h \approx 150 \mu\text{m}$$

$$A \approx 1.53 \text{ cm}^2$$

Ringers for 30 min and then Ringers with fluorescein

Governing Equations

Cell Membrane Flux

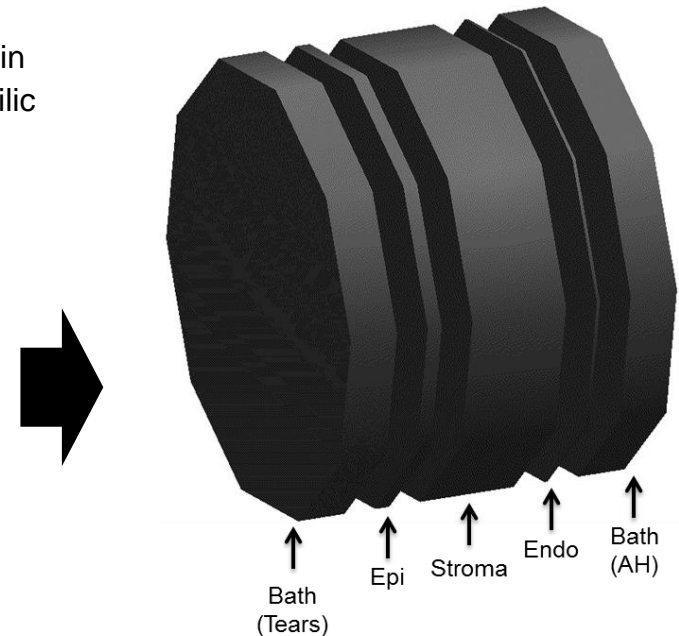
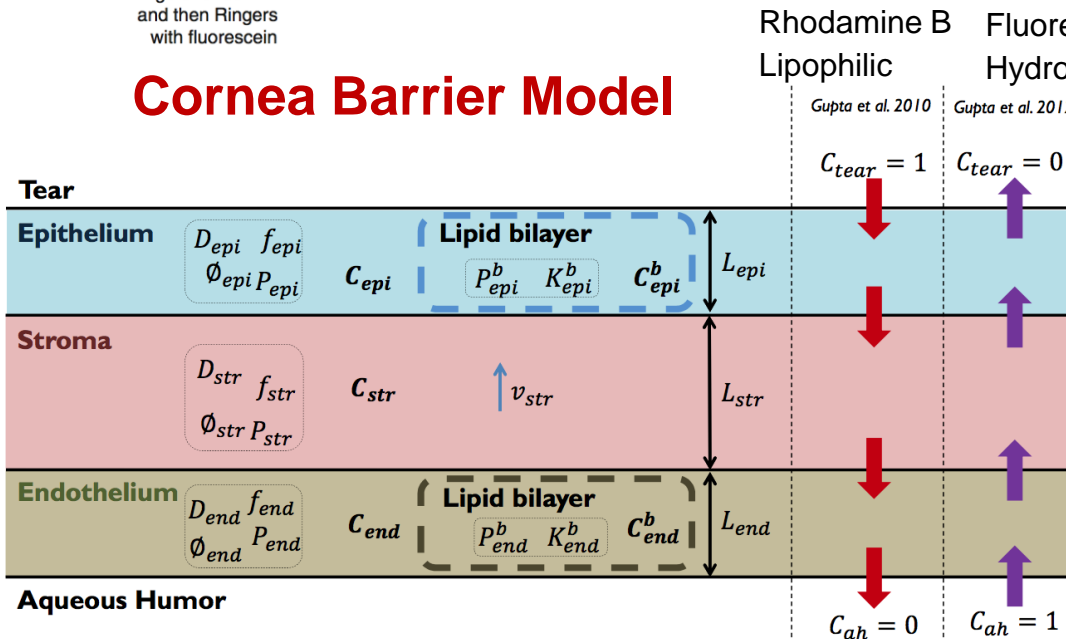
$$J = -D\nabla C - J^B$$

Intracellular Flux

$$J^B = k^B \left(C - \frac{C^B}{R^B} \right)$$

- k^B : cytoplasmic permeability rate constant
- R^B : ratio of equilibrium concentration

Cornea Barrier Model

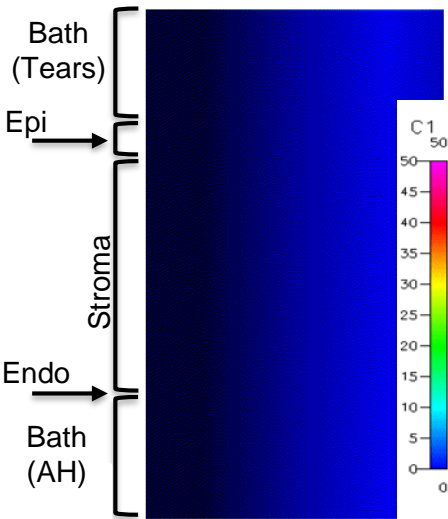


¹Gupta et al (2012). *Pharm. Res.*, vol. 29, no. 12, pp. 3325–3334.

²Gupta et al (2010). *Pharm. Res.*, vol. 27, no. 4, pp. 699–711, Apr.

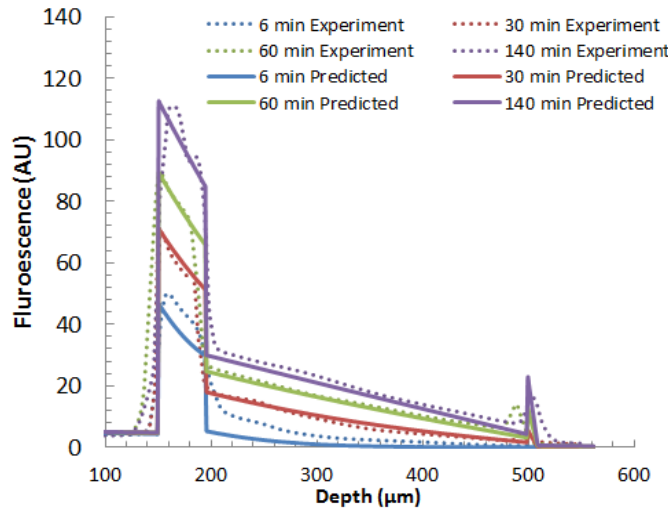
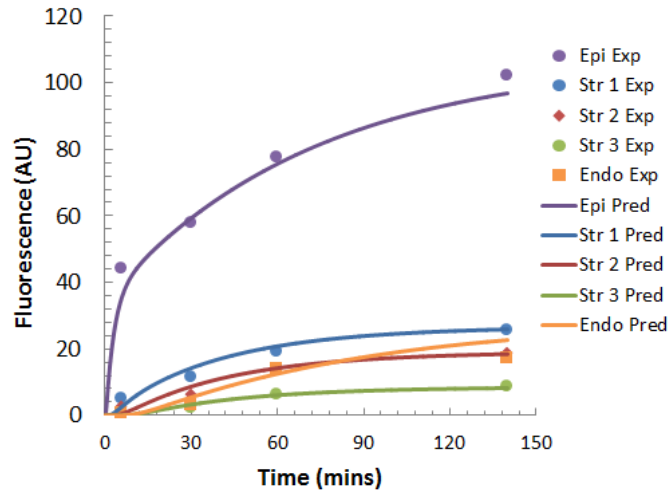
In Vitro/Ex Vivo Validation

Animation



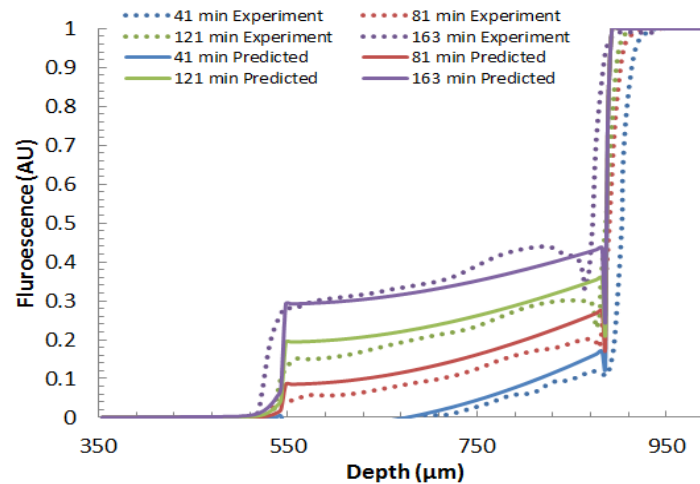
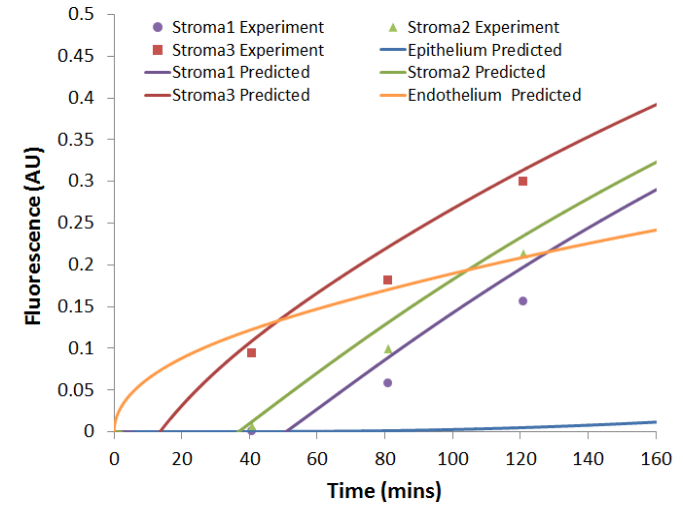
Gupta et al 2010

Rhodamine B

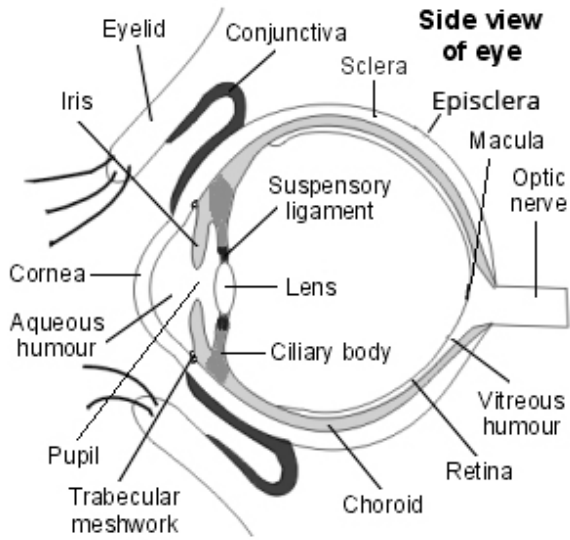


Gupta et al 2012

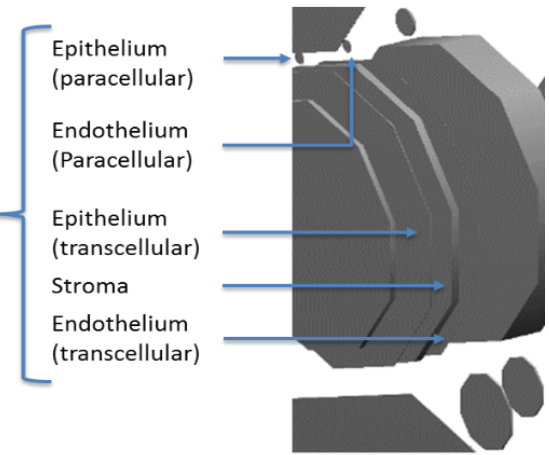
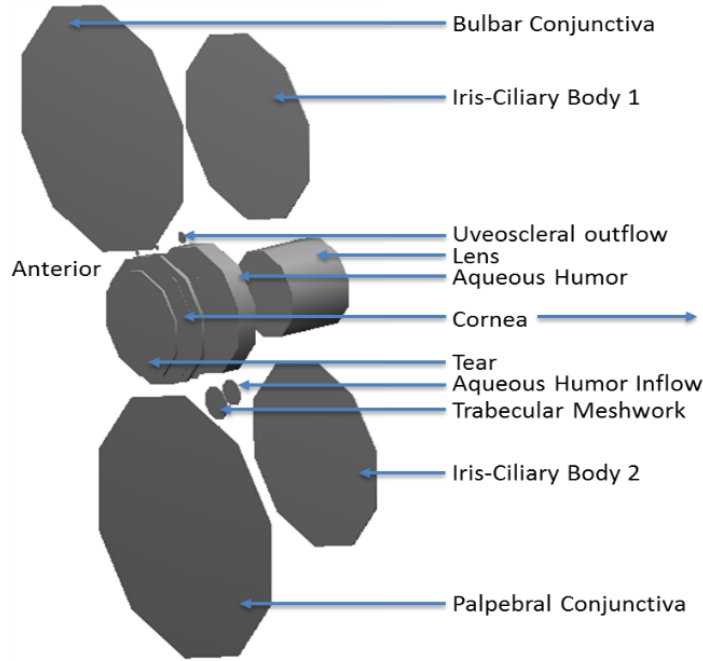
Fluorescein



In Vivo Modeling Approaches: Q3D

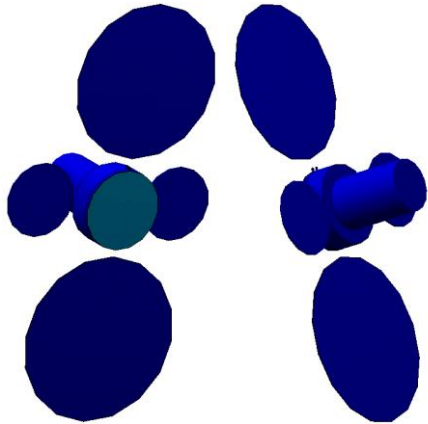


Side view of eye

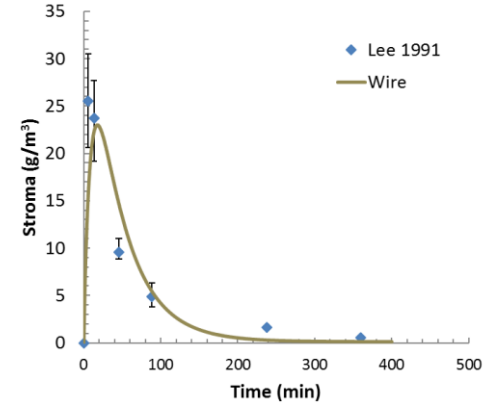
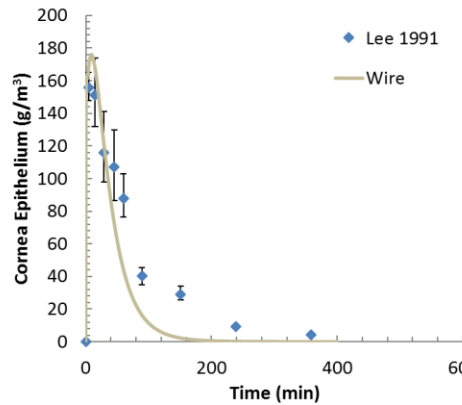
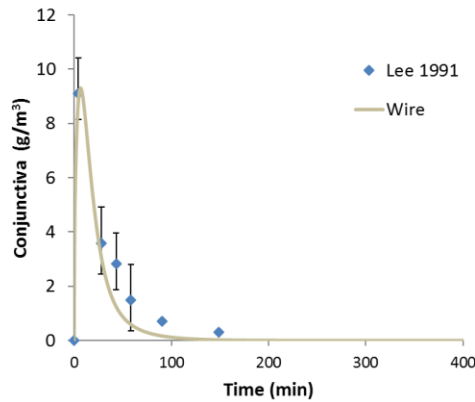


Animation

0.0 Min



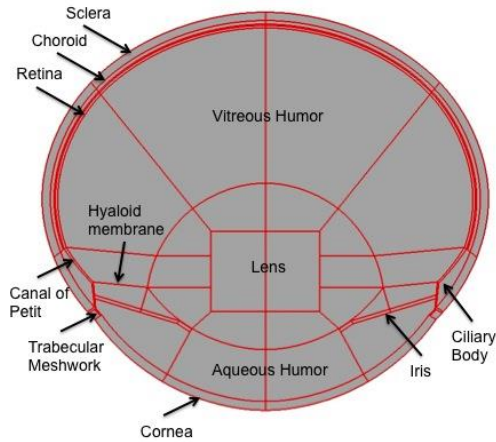
Timolol in the Rabbit Eye



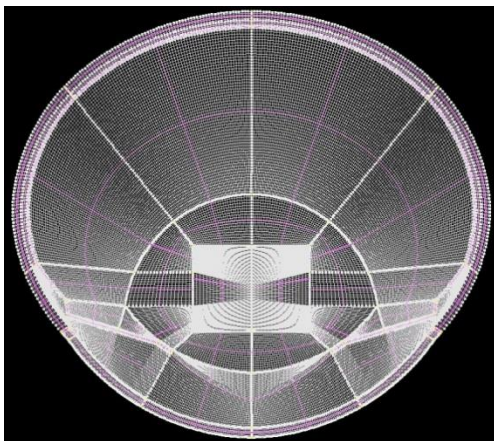
Lee et al (1991) Pharmacokinetic basis for nonadditivity of intraocular pressure lowering in timolol combinations. Invest. Ophthalmology & Visual Sci. Vol.32,2948-2957

In Vivo Modeling Approaches: 2D Axisymmetric

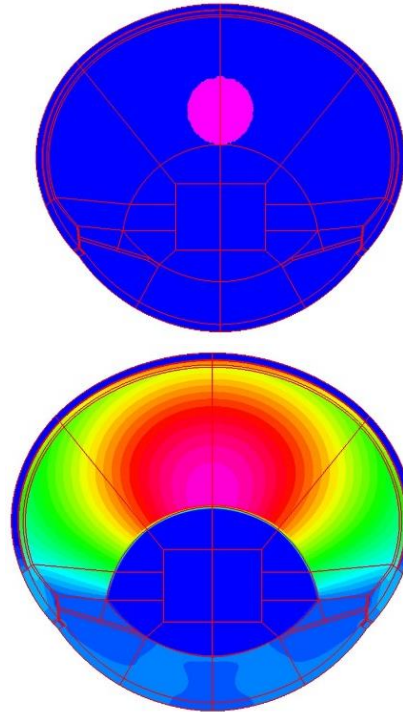
Rabbit Eye Model



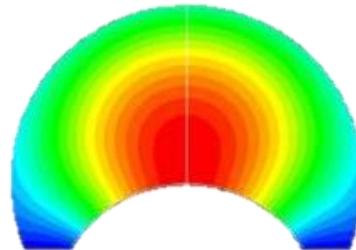
Computational Mesh



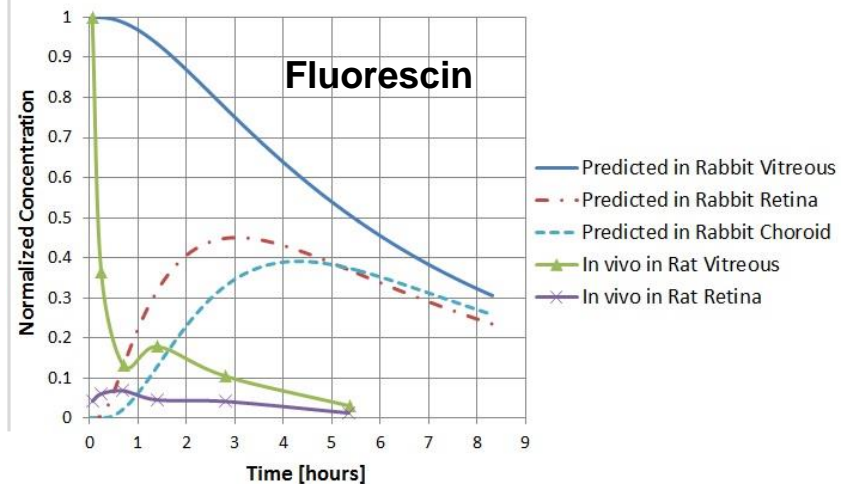
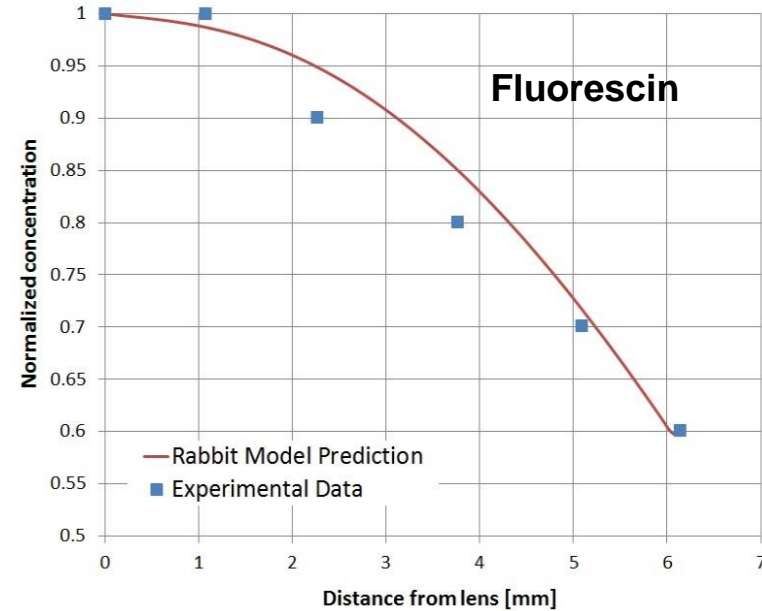
CoBi Predictions



Haghjou et al Predictions

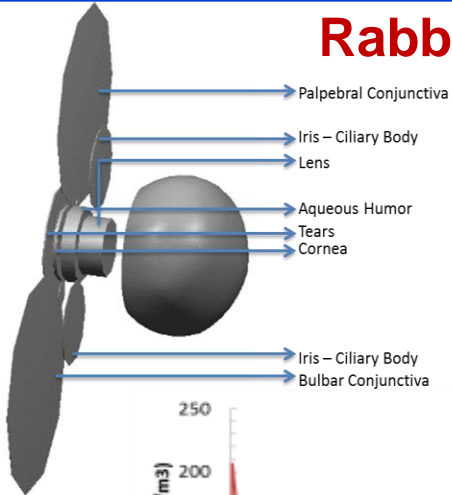


Validation



Whole-Eye Model: Q3D-3D Coupling

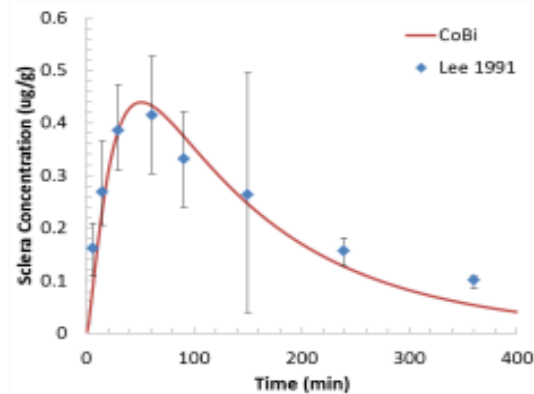
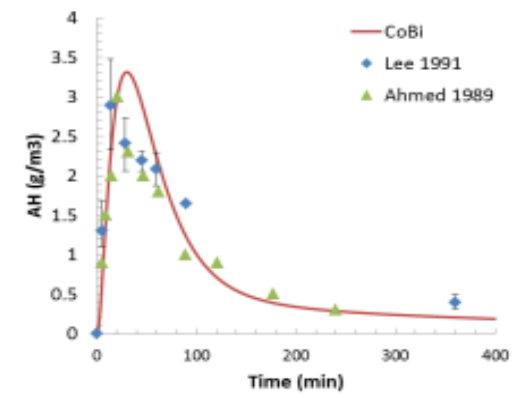
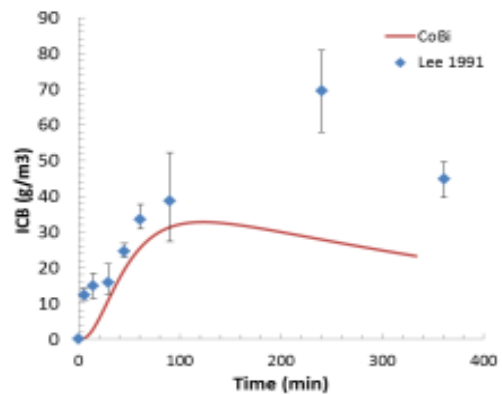
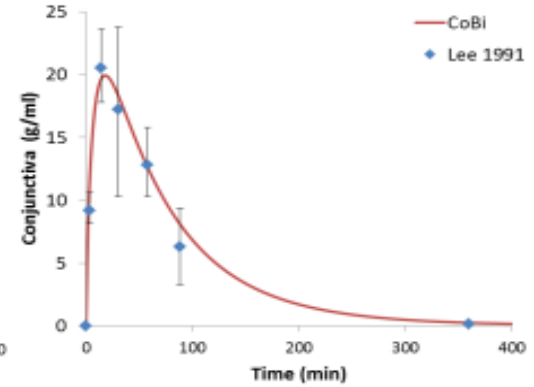
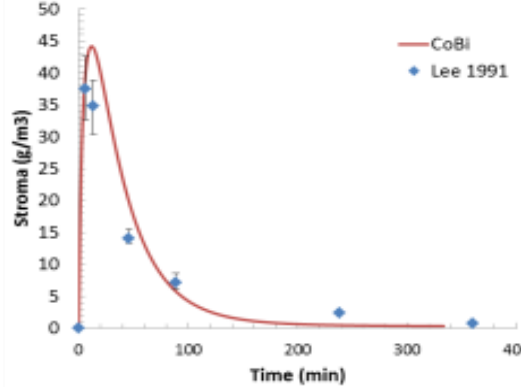
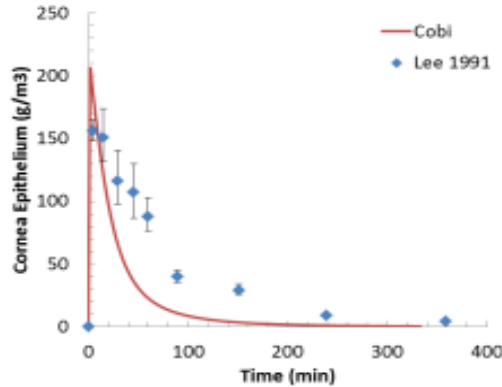
Rabbit Model



Q3D-3D Coupled Model:

- Anterior Eye – Q3D
- Posterior Eye – 3D

PK Profiles - Timolol



Lee et al (1991) Pharmacokinetic basis for nonadditivity of intraocular pressure lowering in timolol combinations. Invest. Ophthalmology & Visual Sci. Vol.32,2948-2957

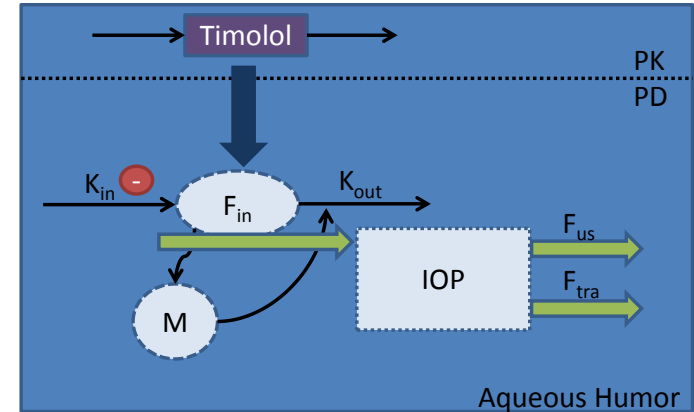
PD model:

- 5 mg/ml instillation of Timolol causes IOP drop
- Increasing Timolol concentration extends duration of IOP drop, but IOP will not dip below ~17.6mmHg due to M regulator

PD Model Parameters

Constant	Value	Description	Units
IC_{50}	5.71E-3	Drug amount needed to inhibit F_{in}	nmol/ml
I_{max}	0.268	Timolol max inhibitory effect	
C_{of}	0.170	outflow facility	$\mu\text{l}/\text{min}/\text{mmHg}$
P_v	9	Episcleral Venous Pressure	mmHg

PD Model Schematic



PD Model Equations

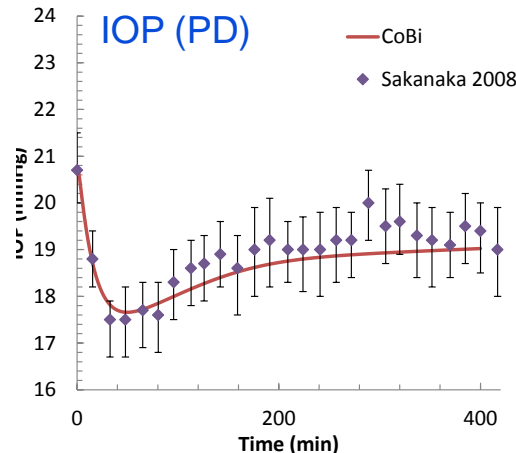
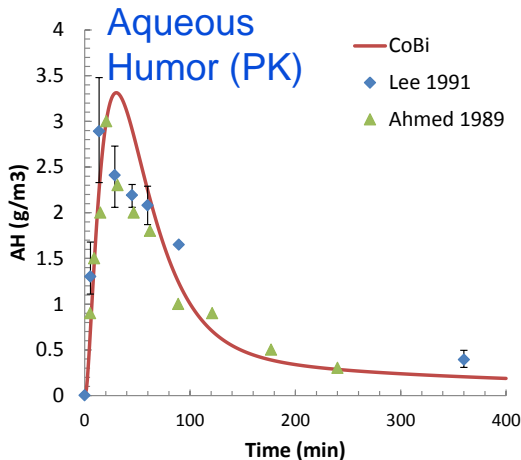
$$F_{tra} = C_{of} (IOP - P_v)$$

$$IOP = P_v + \frac{F_{in} - F_{us}}{C_{of}}$$

$$\frac{dF_{in}}{dt} = K_{in} \left(1 - \frac{I_{max} \cdot C_A}{IC_{50} + C_A} \right) - K_{out} \cdot F_{in} \cdot (1 + M)$$

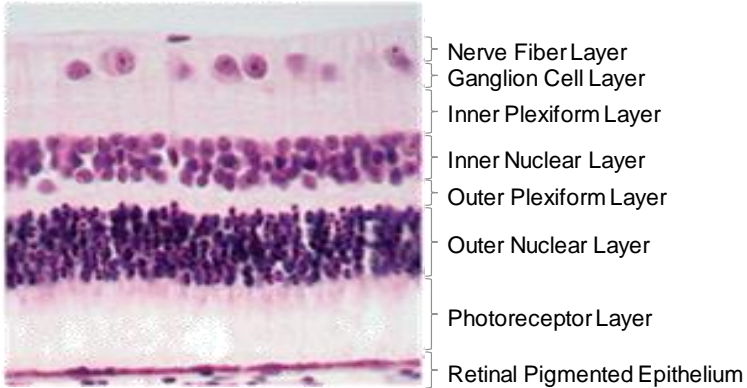
$$\frac{dM}{dt} = K_t (F_{in} - M)$$

$$\frac{dIOP}{dt} = \frac{1}{C_{of}} \left[K_{in} \left(1 - \frac{I_{max} C_A}{IC_{50} + C_A} \right) - K_{out} (F_{tra} - F_{us}) (1 + M) \right]$$



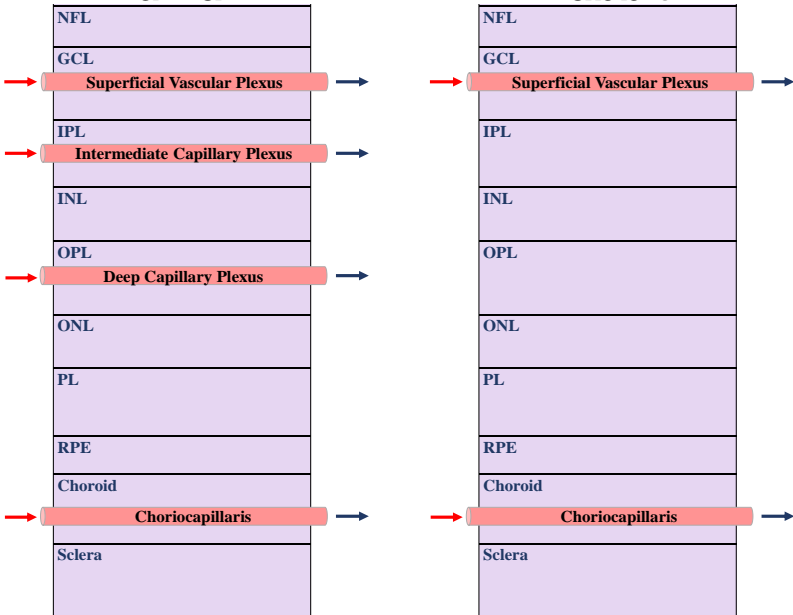
High-Resolution Modeling of the Retina

Anatomy



Human

Rabbit



Model Equations

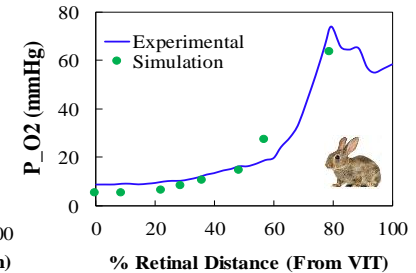
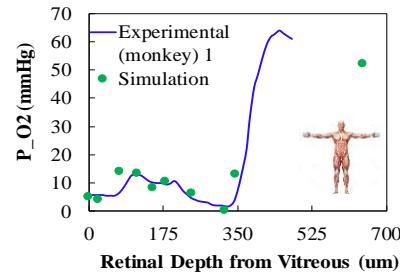
Tissue:

$$\frac{\partial C_i}{\partial t} = J_{D_{i-1_i}} - J_{D_{i_i+1}} + \frac{A_{retina} \cdot \psi_{b-t} \cdot (C_j - C_i)}{V_i}$$

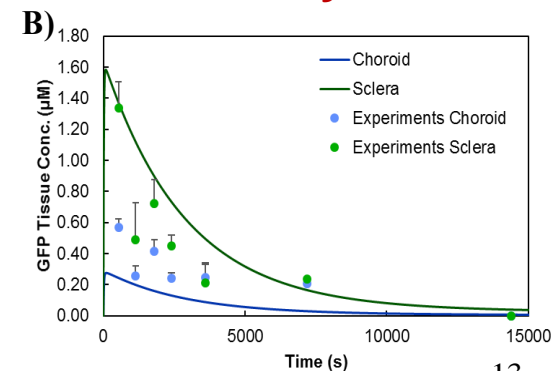
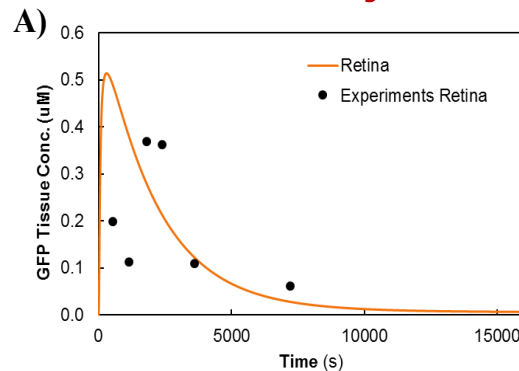
Blood:

$$\frac{\partial C_j}{\partial t} = \frac{Q_j \cdot (0 - C_j)}{V_j} - \frac{A_{retina} \cdot \psi_{b-t} \cdot (C_j - C_i)}{V_j}$$

Oxygenation Profiles



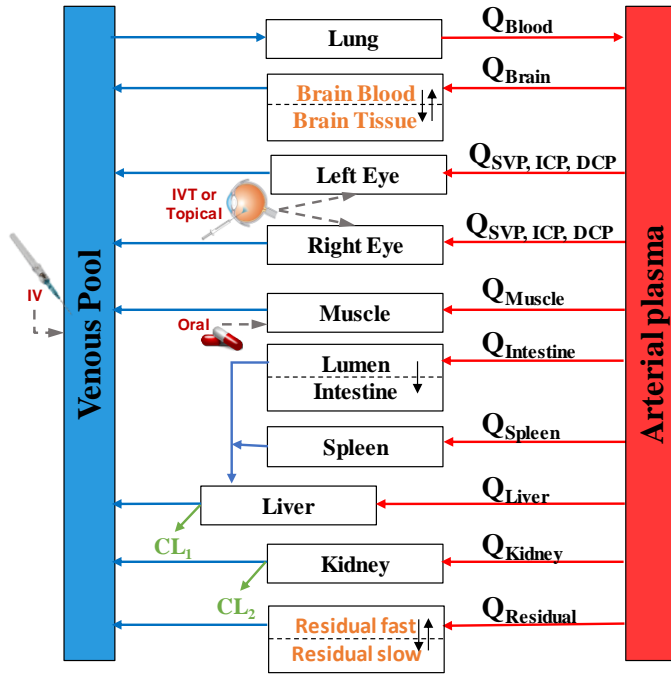
Tracer PK Profiles (GFP) Periocular Injection in the Rabbit Eye



PBPK-High-Resolution Eye Modeling/Validation

Nutlin-3A

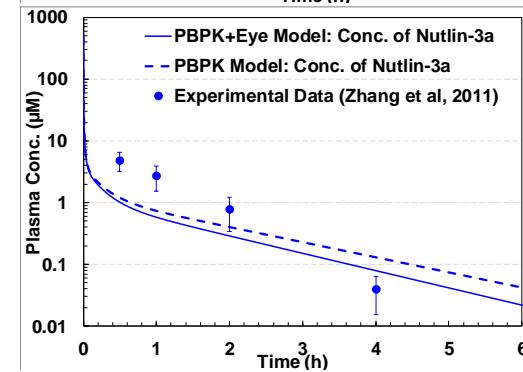
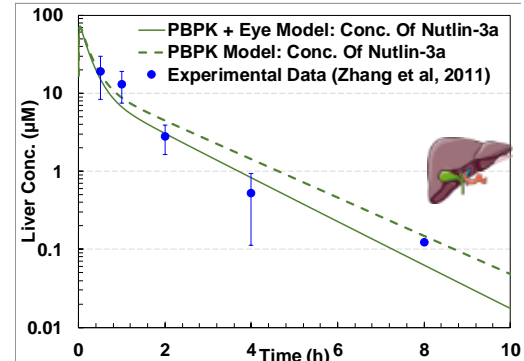
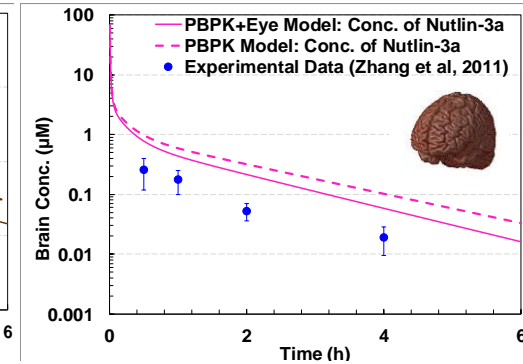
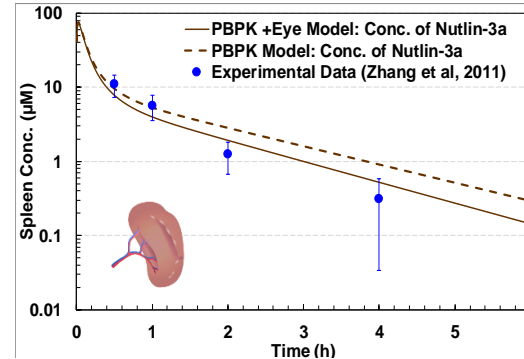
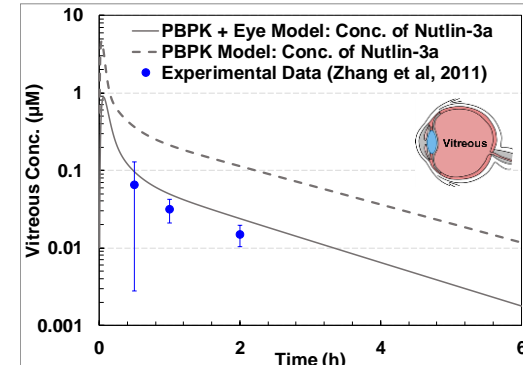
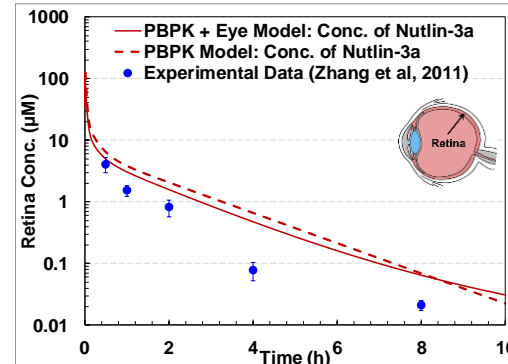
Mouse PBPK Model



Organ Model Eqs.

Perfusion-Limited
$$V_i \cdot \frac{dC_i}{dt} = Q_i \cdot \left(C_{ART_PL} - \frac{C_i}{K_i} \right)$$

Permeability-Limited
$$V_j \cdot \frac{dC_j}{dt} = PA_j \cdot \left(C_i - \frac{C_j}{K_j} \right)$$



Summary and Plans



- Developed components of a multiscale computational framework, CoBi, for modeling in vitro and in vivo ocular drug delivery, PK/PD
- Developed a framework for modeling in vitro dissolution of
 - ophthalmic products (suspensions, micelles, ...) validation in progress
 - dissolution equipment (USP2 USP 4, Transwell,...)
- Developed Q3D models of the anterior eye , posterior eye (retina)
- Performed initial validation of model components

- Ongoing
 - Improves of the Anterior Eye Model (anatomic geometry, tear film)
 - Development and validation of dissolution model for complex drug products
 - Models of Topical Delivery of Suspension Products
 - Integration of the In vitro and In vivo models
 - Development of model based IVIVE

CoBi tools and all models available on Open Source