A MULTISCALE MODELING APPROACH TO OPTIMIZE PULMONARY DRUG DELIVERY Ravi Kannan<sup>1</sup>, Narender Singh<sup>1</sup>, Andrzej Przekwas<sup>1</sup>, Renish Delvadia<sup>2</sup>, Geng Tian<sup>2</sup>, and Ross Walenga<sup>2</sup> <sup>2</sup> FDA, Silver Spring, MD <sup>1</sup> CFDRC, Huntsville, AL;

Can we efficiently use computational tools to capture the experimentally challenging mechanistic insights of pulmonary drug delivery processes?

### INTRODUCTION

**Pulmonary drug delivery** via oral inhalation is being increasingly used for both treatment of lung diseases and for delivering drugs to the systemic circulation.

Efficacy and safety of such orally inhaled drugs is dependent on deposition and absorption of drugs in targeted regions of the lung.



#### SELECTED COMPUTATIONAL PK RESULTS

. The predicted formulation effects of pulmonary drugs on drug particle dissolution for poly-dispersed budesonide (dose = 200  $\mu$ g; Solubility = 17  $\mu$ g/ml; Diffusion coefficient =  $6.2e-6 \text{ cm}^2/\text{min}$ ; Dissolution vol. = 1 L) is shown below:



However, analyzing inhaled pulmonary drug disposition is experimentally challenging as it involves complex mechanisms, such as regional drug deposition, dissolution, transport in lung barriers and mucociliary clearance.

. Here, using multiscale computational tools, our goal is to:

. Develop, evaluate, and improve physiologically-based absorption and pharmacokinetic models of pulmonary (inhaled) drugs; and

. Support the development of generic oral inhaled drug products (OIDPs).

. The **predicted inhaled PK** values for momentasone furoate (MF), budesonide and fluticasone propionate (FP) simulations is shown below:



MF plasma concentration after 400 µg inhalation

Budesonide plasma concentration after 1000 µg

**FP** plasma concentration after 1760 µg inhalation

#### **MULTISCALE COMPUTATIONAL METHODOLOGY**



. The framework employed Typical Path Lung (TPL) & Computational Fluid Dynamics (CFD) models to calculate **lung depositions**. Results presented here are based on TPL models.

To evaluate **dissolution** we employed Noyes-Whitney type equation in any compartment based on dose, solubility, diffusivity, size, and mono/poly-dispersability of the selected drug.

Experimental data-based **mucociliary transport** equation is used to account for the loss of dissolved drug when mucous moves from upper lung 'airways-to-mouth-to-gut'.

The lung-barrier transport/absorption model from Yu et al. is used to predict drug retention/transport across lung tissue from 'epithelial-to-blood'

Finally, whole-body human physiology-based pharmacokinetic model (PBPK) is used to connect pulmonary blood to gut (CAT) model to predict **lung and blood PK** of the drug.

## FDA U.S. FOOD & DRUG

ADMINISTRATION

dose	inhalation dose	dose

#### **FUTURE AND CONCLUSION**

. Our comprehensive multiscale modeling approach can be efficiently used to predict OIDPs PK profiles at multiple lung sites (e.g., in smooth muscle cells [SMC] as shown in figure on right).

. Our approach can be successfully applied in: Dose optimization, effect of drug's physiochemical properties (logP, MMAD, etc.), and ultimately device design and generic drug formulations, if relevant information is available for modeling input.

Attempts to model and compare the drug delivery in disease (reduced diameter) vs. healthy lungs as shown in figure on right.

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# SMC drug conc. at 25 (L) & 250 (R) min's Disease

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