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# The Effects of Mometasone Furoate Formulation Factors and **Actuator Design on Metered Dose Inhaler (MDI) Performance**

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### Purpose

Metered dose inhalers (MDIs) are complex drug-device combination products widely used as portable delivery systems to treat a variety of pulmonary disorders including asthma and chronic obstructive pulmonary disease (COPD). A typical MDI (Figure 1) consists of a canister, a metering valve, and an actuator-mouthpiece.<sup>1,2</sup> The formulation within the cannister containing the active pharmaceutical ingredient (API) can be either the form of a solution (API dissolved in liquid propellant) or a suspension (API particles dispersed in liquid propellant) along with inactive ingredients (e.g., co-solvents and surfactants).

Product performance for MDIs depends on a myriad of factors including formulation characteristics and device design. Formulation factors that can vary include physiochemical properties of the API, and the amount and nature of excipients.<sup>2,4</sup> MDI device geometry can vary including valve metering chamber volume, actuator nozzle orifice diameter, actuator sump depth, and actuator orifice jet length.<sup>2,4</sup> Currently, the impact of formulation factors on MDI performance and its interaction with actuator design is not fully understood. Therefore, the purpose of this work is to investigate how formulation factors along with actuator parameters influence in vitro product performance for mometasone furoate (MF) MDIs.



Figure 1. Schematic of a typical MDI.<sup>2</sup>

## Methods

Formulation of MF MDIs: Three suspension-based MF MDIs were manufactured with changes in API particle size distribution (PSD D50) (Figure 2), oleic acid (OA, surfactant), and ethanol content (EtOH, cosolvent) (Table 1) in HFA-227 propellant. Each of the three MF MDI formulations were characterized for API content, ethanol content, oleic acid content, and moisture content.

Table 1: Formulation characteristics of MF MDIs.								
MF Formulation Characteristics								
Formulation	API PSD D50 (μm)* EtOH (% w/w) OA (% w/w)							
#1	1.69 0.52 0.0043							
#2	#2 1.10 2.10 0.0151							
#3	#3 1.69 1.30 0.0104							
* PSD (Particle Size Diameter) D50: Particle diameter at 50% in the								
cumulative distribution (median diameter)								



Table 2: Actuator variant parameters.

Actuator Parameters						
Actuator Variant	OD (mm) JL (mm)		SD (mm)			
A	0.48	0.6	1.2			
В	0.48	0.4	1.5			
C	0.35	0.6	1.5			
D	0.35	0.4	1.2			





Figure 2. Scanning Election Microscopy images of MF API.

Actuator variants: Four actuator variants (Figure 3) differing in orifice diameter (OD), jet length (JL), and sump depth (SD) were encompassed in the analysis to evaluate formulation-actuator interactions

	Expansion Chamber or Sump Depth SD	Orifice Diamete
Figure 3. Des	sign of MDI actuato	or orifce. <sup>5</sup>

In Vitro Characterization:

The MF MDIs (all 12 combinations of 3 formulations and 4 actuators) were characterized and evaluated by a variety of in vitro tests (below) to assess product performance. Statistical analyses on the data (ANOVA) were conducted to determine the effects of formulation factors and actuator design. **Delivered Dose (DD)** was based on the mass deposited in a CareFusion AirLife EU303 filter (F) following the method described in USP <601>.

Aerodynamic Particle Size Distribution (APSD) was evaluated using a Next Generation Impactor (NGI) with an USP induction port (IP) with coated cups and back-up filter (CareFusion AirLife EU303) added after the micro-orifice collector (MOC). NGI Delivered Dose (NGI DD) was determined as the sum of drug collected by the NGI (IP to F). Calculations of Fine Particle Fraction (FPF<8µm, FPF<5µm, FPF<2µm) included linear interpolation of the cumulative distribution function normalized to NGI DD. Fine Particle Mass (FPM <  $8\mu m$ , FPM <  $5\mu m$ , FPM <  $2\mu m$ ) was calculated by multiplying the mass deposited on NGI with the FPF.

**Ex-Anatomical Throat Mass** was evaluated using a medium size oropharyngeal consortium (OPC) throat model with mass collected on a CareFusion AirLife EU303 filter.

All these in vitro characterization tests (DD, APSD, and Ex-anatomical Throat Mass) were run at a flow rate of 30 L/min.

To characterize the spray and plume, Spray Pattern (SP) Ovality Ratio and Area as well as Plume Geometry (PG) Angle and Width were determined at a distance of 6 cm away from actuator mouthpiece. Ovality ratio = Dmax/Dmin where Dmax and Dmin are the longest and shortest diameters, respectively, that pass through the center of mass/gravity. The PG angle is based on the conical region of the plume extending from a vertex that occurs at or near the actuator mouthpiece.



#### **APSD** Parameters by Actuator Changes

Table 3. Results (p-values) from ANOVA assessing effects by actuator dimensions, by parameter and formulation. Statistically significant p-values < 0.05 are marked red; F#: Formulation, OD: Orifice Diameter, JL: Jet Length, SD: Sump Depth.

Parameter	F#	OD	JL	SD	JL and SD had <u>no</u> statisti
	#1	0.0636	0.0273	0.1985	significant effects on any
Delivered Dose	#2	0.1802	0.1202	0.3408	the assessed APSD
	#3	0.5464	0.0784	0.6124	parameters
	#1	0.4532	0.9195	0.7832	OD had <u>no</u> effect on the L
NGI Delivered	#2	0.6162	0.6683	0.8402	but it had a strong effect
Dose	#3	0.4068	0.6043	0.9246	the plume exiting the three
	#1	0.0025	0.0386	0.5076	(Ex-Anatomical Throat M
	#2	0.0001	0.4214	0.8669	and FPMs)
Inroat wass	#3	0.0001	0.8960	0.5721	• The results were <u>very</u>
	#1	0.0207	0.3881	0.9072	<u>consistent</u> between
FPM < 8 μm	#2	0.0003	0.2621	0.8686	formulations, indicating
	#3	0.0006	0.2767	0.8773	these effects are
	#1	0.0352	0.4065	0.9582	formulation independent.
FPM < 5 μm	#2	0.0014	0.4166	0.8930	The size of the significant
	#3	0.0012	0.4145	0.9969	effects might however di
	#1	0.1338	0.5056	0.7079	between formulations (se
FPM < 2 μm	#2	0.0072	0.9037	0.8084	Table 4).
	#3	0.0199	0.5332	0.5507	



<u>Figure 7</u>. Mean MF deposition by actuator variant on the NGI; AD: Adaptor, ST: Stem, ACT: Actuator, IP: induction Port, S1-S7: Stage 1 Stage 7; MOC: micro-orifice collector F: Filter.

• OD was the most influential actuator characteristic for MF deposition on the NGI. Smaller OD (actuators C and D) allowed for increased deposition on stages S3 and S4, and decreased deposition on the IP.



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<u>Figure 5</u>. (A) FPM < 8µm, (B) FPM <  $5\mu$ m, and (C) FPM <  $2\mu$ m for 3 formulations and 4 actuator variants (mean ± \*p<0.05, ANOVA: **Fukey's Multiple Comparison Test); MF:** Mometasone Furoate, F1: Formulation #1, F2: Formulation #2, and F3: Formulation #3.

- Statistical differences in formulations were seen in FPM < 8 µm and FPM < 2 µm, but <u>not</u> in FPM < 5 µm, using the same actuator variant.
- No statistical changes were seen between Formulation #1 and Formulation #3 for FPMs, which suggests that OA and EtOH concentrations may not significantly impact FPM.
- A lower API PSD in Formulation #2 most likely accounts for increased extra fines (FPM < 2 μm).



Figure 6. Mean MF deposition by formulation on the NGI; AD: Adaptor, ST: Stem, ACT: Actuator, IP: induction Port, S1-S7: Stage 1- Stage 7; MOC: micro-orifice collector; F1: Formulation #1, F2: Formulation #2, F3: Formulation #3.

- Formulation #2 had significantly extra fine particle mass (FPM < 2 µm) compared to Formulations #1 and #3, allowing for differences in MF deposition on the lower NGI stages and suggesting that lower API PSD in Formulation #2 may P and decrease on adaptor and stage S3 were seen for Formulation #3 compared to influence MF deposition.
- Increase in MF deposition on Formulation #1 suggesting that ~ 2fold increase in OA and EtOH may inhibit MF deposition.

Table 4. Least Square (LS) Means (µg) for each actuator dimension and factor level, by parameter and formulation. Statistically significant effects are marked red; F#: Formulation, **OD:** Orifice Diameter, JL: Jet Length, SD: Sump Depth.

		OD		JL		SD	
Parameter	F#	0.35	0.48	0.4	0.6	1.2	1.5
		mm	mm	mm	mm	mm	mm
	#1	179.1	185.5	178.3	186.3	184.4	180.2
Delivered Dose	#2	194.8	189.6	189.1	195.3	194.0	190.4
	#3	185.8	187.8	183.7	190.0	186.0	187.6
NGI Delivered Dose	#1	162.5	158.1	160.0	160.6	159.5	161.1
	#2	151.4	146.7	151.0	147.1	150.0	148.1
	#3	164.7	159.9	160.8	163.8	162.0	162.6
Ex-Anatomical	#1	55.4	43.7	52.9	46.2	50.5	48.6
Throat Mass	#2	<b>59.0</b>	43.1	52.0	50.0	51.2	50.8
Throat Wass	#3	53.0	39.7	46.4	46.2	46.9	45.8
	#1	108.2	95.0	103.7	99.5	101.3	101.9
FPM < 8 μm	#2	100.9	80.9	92.9	88.8	91.1	90.6
	#3	104.8	88.3	98.3	94.7	96.8	96.3
	#1	79.3	68.9	75.9	72.3	74.0	74.2
FPM < 5 μm	#2	84.1	67.4	77.2	74.2	76.0	75.5
	#3	77.1	65.4	72.3	70.2	71.2	71.2
	#1	9.0	7.7	8.6	8.1	8.2	8.5
FPM < 2 μm	#2	17.1	13.2	15.3	15.1	15.0	15.3
	#3	9.0	7.6	8.1	8.5	8.2	8.5

- The statistically significant effects by OD were in the range of 14-37%\*, with larger results for the smaller OD of 0.35 mm. • The numerically strongest effect was seen on the Ex-
- Anatomical Throat Mass (range of 27-37%\*). The results are consistent between formulations but with a
- clearly stronger effect on Formulation #2 (range of 25-37%\*) as compared to Formulation #1 (range of 15-27%\*) and Formulation #3 (range of 14-34%\*). This may indicate that design and control of the spray OD is more critical for suspension-based MDIs with finer APIs.
- \* Calculation as follows: [ (LS mean of smaller parameter LS mean of larger parameter) / (LS mean of larger parameter) x 100%].

#### **Spray Pattern and Plume Geometry**

Table 5. Results (p-values) from ANOVA of SP and PG results. Statistically significant p-values < 0.05 are marked red

Endpoint	Formulation	OD	JL	SD			
SP Ovality	0.0493	0.2499	0.5444	0.0155			
SP Area	0.0000	0.0949	0.0000	0.5158			
PG Angle	0.0060	0.6904	0.0000	0.0180			
PG Width	0.0733	0.9371	0.0006	0.1126			

#### Effects on Spray Pattern Area



**Figure 8. SP Area Changes by Formulation and** Jet Length.

- Table 5 shows that formulation and JL were statistically significant on almost all the SP and PG endpoints. OD had no statistically significant differences.
- Figure 8 shows that SP area demonstrated the largest change of all SP and PG endpoints, which was most affected by formulation and JL. SP area was reduced by 10-15% when JL increased. Formulation #2 had largest SP area (~12-15% larger) compared to #1 and #3.
- Of all SP and PG endpoints, SP area was seen to <u>correlate (but not very well)</u> with several APSD parameters including delivered dose (DD) and mass median aerodynamic diameter (MMAD), as calculated by Pearson's correlation coefficient (|r| > 0.6).



## Conclusions

- Statistical differences in formulations were seen in DD and Ex-Anatomical
- Throat Mass and were most apparent when using Actuator Variant D. Formulation #2 had significantly extra fine particle mass (FPM < 2µm)</li> compared to Formulations #1 and #3, allowing for increased MF deposition on the lower NGI stages, which is most likely due to lower API PSD in Formulation #2.
- The influence of OA and EtOH warrant further investigation to understand their specific impacts on MF MDI aerosol performance.
- JL and SD had no effect on MF MDI APSD testing within the ranges studied
- OD had no effect on DD but a strong effect on plume exiting the throat (FPMs and Ex-Anatomical Throat Mass) and is formulation independent.
- The change in OD led to statistical significant effects in FPMs and Ex-Anatomical Throat Mass, ranging 14-37% for all formulations. OD had stronger effect on Formulation #2 compared to Formulations #1 and #3, which indicates that control of OD may be more critical for formulations with finer APIs (lower API PSD).
- Formulation and JL are most influential on the SP and PG endpoints. Specifically, SP area demonstrated the largest change of all SP and PG endpoints determined. SP area was reduced by 10-15% when JL increased. Formulation #2 had ~12-15% larger SP area compared to formulations #1 and #3.
- SP area was seen to correlate slightly with several APSD parameters including delivered dose (DD) and mass median aerodynamic diameter (MMAD) through Pearson's correlation coefficient (|r|>0.6).
- Overall, formulation factors and actuator design have shown to influence in vitro product performance of suspension-based MF MDIs. The possible effects of varying these characteristics must be studied on a case-by-case
- Results from this work allow for improvement in quality by design (QbD) approaches to streamline MDI drug product development (both brandname products and their generic counterparts) and provide insights on how to control MDI drug product performance parameters to achieve a desired performance profile.

### References

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