

Validation of computational predictions of regional lung deposition

Bo Olsson

Emmace Consulting AB, Lund

September 30, 2021

Disclaimer

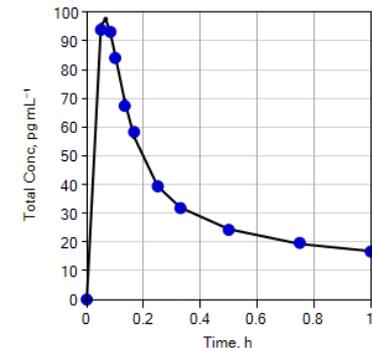
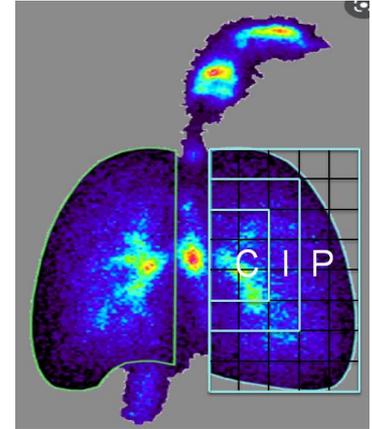
- I am a consultant for Emmace Consulting AB, Lund, Sweden, and I work with many pharmaceutical companies on inhalation science.
- I am also a majority shareholder of Mimetikos AB, owner of the Preludium™ software.

Background

- **Computer models of lung deposition are important**
 - For predicting and/or understanding clinical studies.
 - For facilitating development of inhalation products.
- **Validation of such models is challenging**
 - Must be indirect since generational *in vivo* data are lacking.
 - Hence, no direct records to compare with.
 - Hence, either *in vivo* data or *in silico* predictions must be transformed for them to become comparable.
 - This require assumptions.

Validation approaches to be discussed:

- **Planar scintigraphy**
 - The most common type of *in vivo* data addressing lung deposition.
 - Provides an image where each Region of Interest, RoI (e.g., central, intermediate and peripheral), contains a mixture of airway generations.
 - Hence, one cannot directly compare, say predicted deposition in generations 1-8 with the activity recorded in the central region of the image.
- **Pharmacokinetics (C vs t plasma curve, C_{max}, AUC, etc)**
 - Downstream biomarkers, even more indirect.
 - Based on different regions having different rate and/or extent of absorption.
 - Requires mechanistic model for absorption from lung into system.
 - Which in turn requires validation.



Planar scintigraphy vs Generational deposition

- Each RoI captures activity in a mixture of generations
 - Not possible to translate RoI activity to generational deposition (fuzzy → detailed).
 - Possible to translate generational deposition to RoI activity (central, C, intermediate, I and peripheral, P) (detailed → fuzzy).
 - Requires a translation map.
 - Such a map has been published by Schroeter et al*, based on a 2D projection of a 3D mathematical model of a lung.
 - Essentially this downgrades generational deposition to a blurred image.
 - Captured and computed RoI can be directly compared.

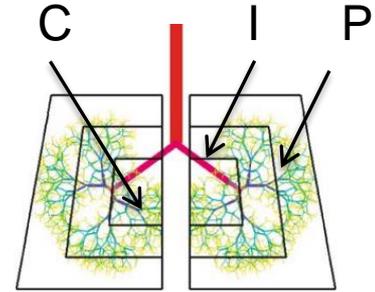


Fig. 4. Planar view of the 3-D airway morphology model (generations 0–12) with overlaid partition.

| Generation | Region of interest | | |
|------------|--------------------|------|------|
| | C | I | P |
| 1 | 100.0 | 0.0 | 0.0 |
| 2 | 100.0 | 0.0 | 0.0 |
| 3 | 50.0 | 50.0 | 0.0 |
| 4 | 50.0 | 50.0 | 0.0 |
| 5 | 25.0 | 75.0 | 0.0 |
| 6 | 25.0 | 50.0 | 25.0 |
| 7 | 25.0 | 50.0 | 25.0 |
| 8 | 20.3 | 54.7 | 25.0 |
| 9 | 18.8 | 49.2 | 32.0 |
| 10 | 19.1 | 43.8 | 37.1 |
| 11 | 18.6 | 39.8 | 41.6 |
| 12 | 18.0 | 39.3 | 42.8 |
| 13 | 17.7 | 39.6 | 42.7 |
| 14 | 17.7 | 38.8 | 43.4 |
| 15 | 18.0 | 38.2 | 43.8 |
| 16 | 18.0 | 38.3 | 43.7 |
| 17 | 18.1 | 38.1 | 43.7 |
| 18 | 18.1 | 38.0 | 43.8 |
| 19 | 18.2 | 38.0 | 43.8 |
| 20 | 18.2 | 38.1 | 43.8 |
| 21 | 18.2 | 38.1 | 43.7 |
| 22 | 18.2 | 38.1 | 43.7 |
| 23 | 18.2 | 38.1 | 43.7 |

* Schroeter et al 2005: Pharm Res 22(10)1692

Mimetikos Preludium™ software

- 1D typical path semi-mechanistic algorithms for generational deposition by impaction, sedimentation and diffusion.
- Inputs: Particle size distribution (MMAD, GSD, Coarse fraction), lung morphology (e.g., scaled Weibel), aerosol transport (e.g., bolus), ventilation (e.g., unsteady breathing pattern), disease (e.g., bronchoconstriction).
- Output: generational deposition, deposition in RoI (using Schroeter map).

Model Specification - 7D15FD22

Deposition model

Extra-thoracic: Fixed
Value (%): Coarse 85.0
Thoracic: NCRP

Lung model

Browse: LungModels
Anatomy: <Weibel17>
Hash: B5043E71
Open Lung design fom
Lung volume at FRC (mL): 3300
Extra-thoracic volume (mL): 50.0
Disease model:

Transport model

Tidal aerosol
 Bolus aerosol
Bolus volume (mL): 500
Delay volume (mL): 0
Fit flow curve
Fit bolus
Show breath info:

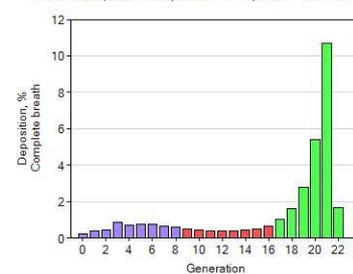
Ventilation model

L min⁻¹ mL s⁻¹ Exp=Insp
Tidal volume (mL): 1600
Peak Inspiratory flow rate: 39.0
Breath hold time (s): 2.0
Peak Expiratory flow rate: 39.0
Use Breath model:
Peak time (s): 1.00
Peak duration (s): 0.00

Breath info

I+B+E (s) = 3.87+2.00+3.87 = 9.73
Minute volume (L min⁻¹) = 9.9
Breathing frequency (min⁻¹) = 6.2
Ave. flow rate I:E (L min⁻¹) = 24.8:24.8

MMAD=3.209, GSD=1.546, Coarse=67.73, sHash=9684A10F



Rol

Map: <Schroeter>

Inverse P/C

C (%Th*) 24.14
I (%Th*) 39.60
P (%Th*) 36.25
P/C 1.50

Validation - scintigraphic data*

- Considered all papers from Newman and co-workers 1981-2007 (n=37) as collated by Clark** (largest collection using consistent methodology & RoI definition).
- Retained those with sufficient information and technique to allow reliable *in silico* predictions and where *in vitro* (impactor measurement) and *in vivo* (scint study) conditions were similar (e.g., PIF).
- Culled data comprised 14 papers with 18 study legs on 9 DPI*** brands.
 - 11 healthy volunteer and 7 mild-moderate asthmatic legs (8-14 subjects per leg).
- Mouth-throat (MT) deposition, total lung deposition (TLD), and mapped C, I, P fractions were computed in Preludium and compared to corresponding *in vivo* results (average for study leg).

* Olsson & Kassinos 2020, JAMPDD DOI: [10.1089/jamp.2020.1620](https://doi.org/10.1089/jamp.2020.1620)

** Clark 2012, JAMPDD 2012;25(4):179-187

*** Due to non-biorelevant impactor tests, MT deposition and PSD could not be reliably estimated for pMDIs, hence excluded

Scintigraphic validation – Results MT & TLD

In silico and *in vivo* measures correlate with an almost one-to-one relation over a wide range ($R^2 > 0.90$, $p < 0.0001$).

| Grand mean | MT (%DD) | TLD (%DD) |
|------------|----------|-----------|
| In vivo | 67.9 | 31.4 |
| In silico | 62.3 | 36.9 |

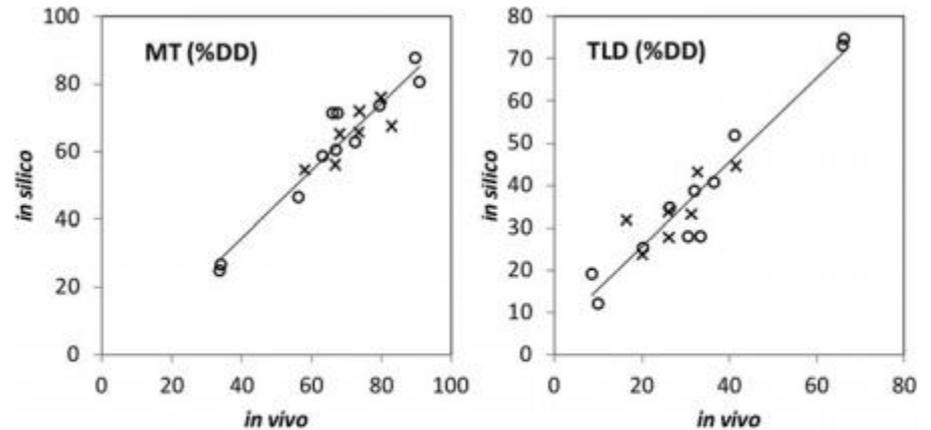


FIG. 1. Unweighted linear regression of *in silico* on *in vivo* results for MT and TLD, % delivered dose. Healthy volunteers (O) and asthmatics (X). MT, mouth-throat; TLD, total lung deposition.

Scintigraphic validation – Results C, I, P & P/C

Significant correlation for P/C ($R^2=0.39$, $p<0.01$) but *in silico* predicted a somewhat less central deposition than *in vivo*.

C somewhat underpredicted, I somewhat overpredicted → P close, slightly overpredicted.

| Grand mean | C | I | P | P/C (range) |
|------------|----|----|----|-----------------|
| In vivo | 34 | 34 | 33 | 1.2 (0.6 – 2.0) |
| In silico | 25 | 40 | 36 | 1.5 (0.8 – 2.1) |

Note: average ratio ≠ ratio of averages

Possible *in silico* P/C range = 0.0 – 2.4.

Possible *in silico* I range = 38 – 41 → the Schroeter mapping is misspecified to some degree.

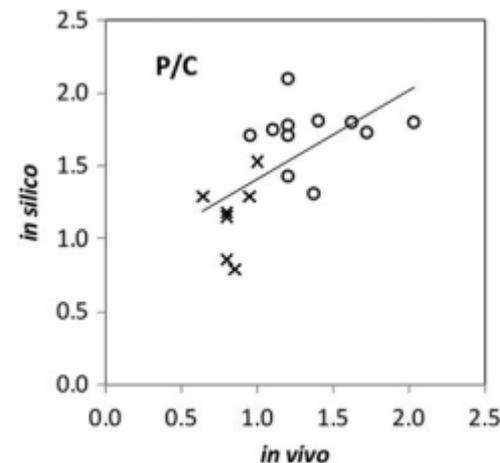


FIG. 3. Unweighted linear regression of *in silico* on *in vivo* results for the P/C ratio. Healthy volunteers (O) and asthmatics (X).

Scintigraphic validation – Conclusion & reflection

- Using an unbiased collection of 18 study legs of DPI deposition and one example of a generation to RoI mapping:
- *In silico* predicted mouth-throat and total lung deposition was highly correlated to *in vivo* outcome with virtually no bias over a wide range.
- *In silico* predicted regional lung distribution was correlated to *in vivo* outcome with a bias towards underestimating central deposition.
- The regional bias is due to a misspecification in the Schroeter mapping to RoI, and possibly also in the Weibel morphological lung model used in Preludium.
- However, a direct comparison of computed alveolar/tracheobronchial (A/TB) deposition ratio with the *in silico* P/C results gave a much larger bias (average 4.2 vs 1.5) demonstrating the necessity of making a translation to comparable measures.

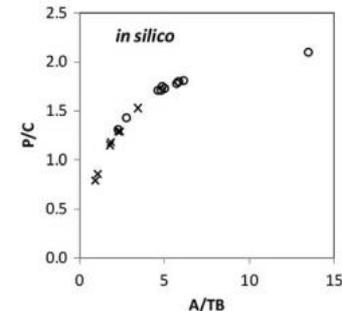
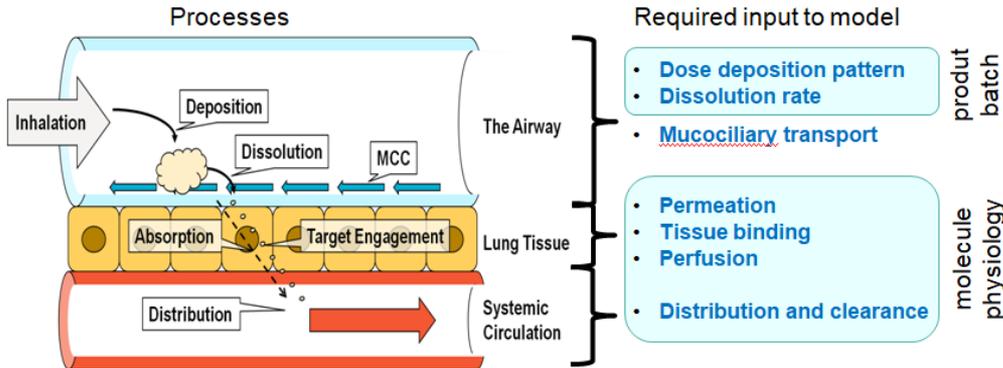


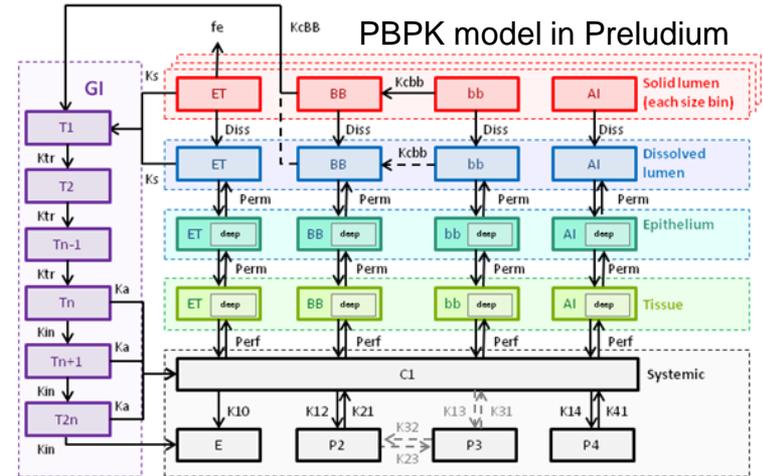
FIG. 4. Relationship between the *in silico* ratios P/C and A/TB. Healthy volunteers (O) and asthmatics (X).

Validation – PK example

- Systemic PK is downstream lung deposition
- Requires mechanistic modeling of pulmonary processes and a systemic model
- Significantly more input parameters and assumptions than for just deposition
- Case study: Fluticasone propionate via Advair® Diskus®



Modified from Olsson and Bäckman, Respiratory Drug delivery 2014



- Pulmonary processes by mechanistic simulation
- Rest-of-body processes by empirical (compartmental) modeling

Validation – Fluticasone proprionate *in vitro* data

- Three strengths of Advair Diskus 100/50, 250/50 and 500/50 (FP/SX).
- Concurrent *in vivo** and *in vitro*** data (same batches similar age).
- Very similar Particle Size Distribution (PSD).
- Marked differences in dissolution rate.

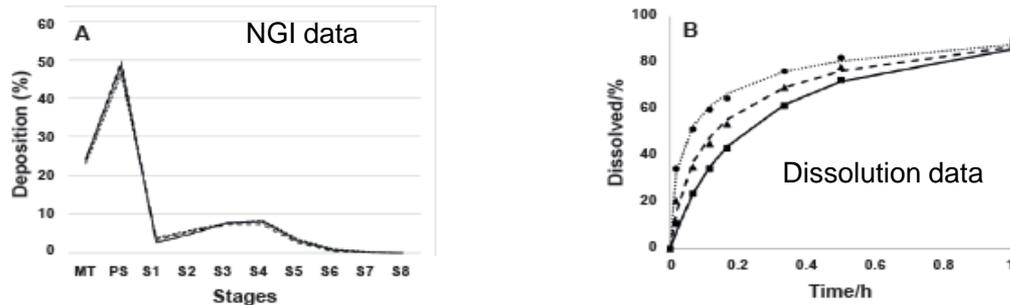


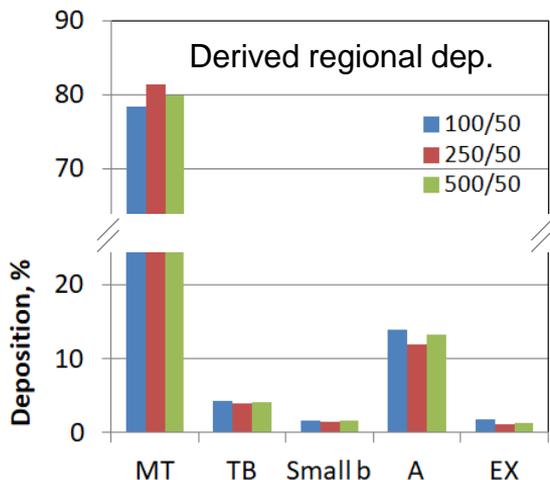
Figure 1. (A) NGI stage deposition (% emitted dose) and (B) actual (data points) and fitted (lines) dissolution profiles of FP from Advair Diskus 100/50 (FP/SX; circles, dotted); 250/50 (triangles, dashed) and 500/50 (squares, solid). Table 1 shows the parameters derived from these data. MT and PS are the USP inlet throat and preseparator, respectively. Dissolved amount is expressed as % of total FP mass added to bath.

* Haughie et al 2020, JAMPDD 33(1)34 (part of ANDA submission for Wixela® Inhub®)

** Bäckman & Olsson 2020, Respiratory Drug Delivery 2020. Volume 1, 113-122

Validation – Fluticasone proprionate *in silico*

- NGI + HV morphometry & maneuver → Total and regional lung deposition.*
- Dissolution curves (dissolution bath, solubility) → VMD_{app} , GSD_{app} .
- Very similar predicted deposition.
- Marked difference in dissolution parameters.



Derived dissolution parameters

| Product | VMD_{app} | GSD_{app} |
|---------|-------------|-------------|
| 100/50 | 2.76 | 3.39 |
| 250/50 | 4.10 | 2.38 |
| 500/50 | 5.08 | 1.85 |

All other model parameters from literature

Validation – FP *in silico* vs *in vivo* PK results

- Similarity in lung deposition manifested in near constant dose-normalized AUCt.
- Difference in dissolution kinetics manifested in trending Cmax and curve shape (Cmax/AUCt).
- Excellent agreement between observed and simulated PK.
- Successful validation of *in silico* model.

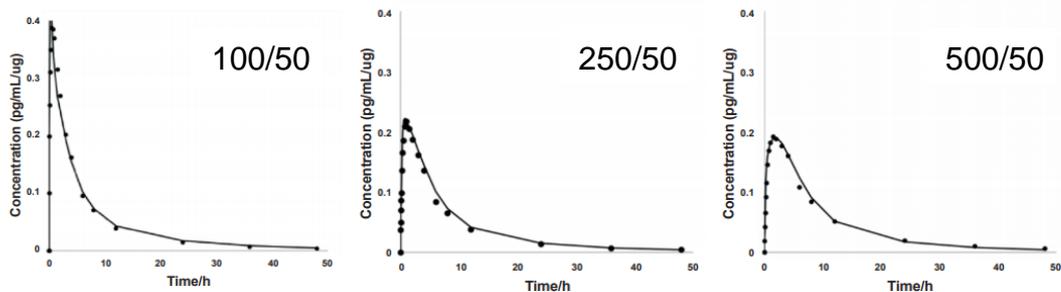


Figure 2. Simulated (solid lines) and observed (markers) dose-normalized plasma concentration versus time for FP following dosing from Advair Diskus (A) 100/50; (B) 250/50; and (C) 500/50 (FP/SX). Simulated and observed concentrations were normalized by division by the total delivered dose in each study.

| Product | Observed* | | | Simulated** | | |
|---------|-----------|-------|-----------|-------------|-------|-----------|
| | AUCt# | Cmax# | Cmax/AUCt | AUCt# | Cmax# | Cmax/AUCt |
| 100/50 | 2.03 | 0.40 | 0.19 | 2.10 | 0.41 | 0.19 |
| 250/50 | 1.65 | 0.23 | 0.14 | 1.80 | 0.21 | 0.12 |
| 500/50 | 1.95 | 0.19 | 0.10 | 1.95 | 0.18 | 0.09 |

Dose normalized by nominal dose

| Product | Simulated/Observed** | | |
|---------|----------------------|------|-----------|
| | AUCt | Cmax | Cmax/AUCt |
| 100/50 | 1.04 | 1.04 | 1.00 |
| 250/50 | 1.09 | 0.92 | 0.85 |
| 500/50 | 1.00 | 0.94 | 0.94 |

* Haughie et al 2020, JAMPDD 33(1)34

** Bäckman & Olsson 2020, Respiratory Drug Delivery 2020. Volume 1, 113-122

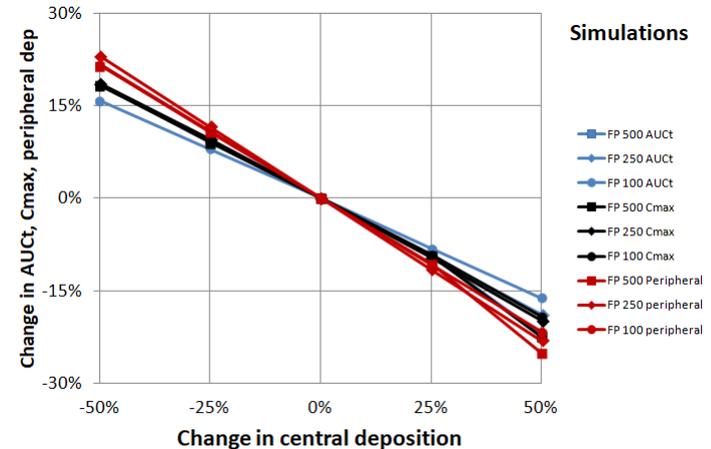
Validation – sensitivity of FP PK to regional deposition

- The simulated central deposition was changed by up to $\pm 50\%$, adding or subtracting to/from the peripheral deposition.
- The resulting changes in AUCt, Cmax, and peripheral deposition show:

- Changes are pronounced and proportional to changes in central deposition
- Changes in AUCt and Cmax closely follow changes in peripheral deposition

- Interpretation

- Changes in Cmax mainly due to more rapid absorption from periphery
- Changes in AUCt mainly due to loss by mucociliary clearance from central but not from peripheral deposition



- The successful validation of the PK model indicates that the deposition and dissolution models are valid

Conclusions

- **Scintigraphy**
 - The validity of mapping generational deposition to 2D scintigraphic RoI was demonstrated.
 - The 2005 Schroeter map can probably be improved with novel space-filling algorithms based on new high-resolution CT data on central airway morphometry.
 - Direct comparison of generational deposition to scintigraphic RoI is an invalid approach.
- **PK**
 - For a low solubility compound dissolution may be rate-limiting for absorption from the lung.
 - This was successfully modeled for three strengths of Advair Diskus using appropriate parameterization (VMD_{app} & GSD_{app}).
 - Sensitivity analysis demonstrated a pronounced influence of regional distribution on PK output indicating validity of the deposition and dissolution models.